The present invention provides therapeutic formulations, including therapeutic nanoemulsions, and related methods for the in vivo delivery of hydrophobic compounds, including an important class of hydrophobic anesthetics. Formulations and methods of the invention include semifluorinated block copolymers and perhalogenated fluorous compounds, such as perfluorooctyl bromide or perfluorodecalin, capable of forming a stable nanoemulsion without the need of conventional lipid components that support bacterial and/or fungal growth (e.g., soybean oil and similar lipids). In certain embodiments, emulsion-based formulations are provided that are capable of formulating, delivering and releasing amounts of hydrophobic drugs effective for a range of clinical applications, including inducing and maintaining anesthesia in patients. In certain embodiments, emulsion-based formulations are provided that are capable of supporting controlled release, for example, over a range of rates useful for clinical applications including rapid and sustained release.
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Hydrophilic Block

Hydrophobic Block

Fluorophilic Block

Perhalogenated Fluorous Additive

Hydrophobic Drug

FIG. 1
Propofol vs B8 vs L3

FIG. 3

FIG. 4

Propofol y = 67.023x - 307.53
B8 y = 51.655x - 280.22
L3 y = 67.929x - 339.27
FIG. 5

Average Particle Size (nm)

Time (d)

FIG. 6

Mean Diameter (nm)

Time (d)
FIG. 7

- Diprivan
- L3
- B8
- F8

Log(mg/kg) dose vs. RORR (s)
Slopes:

Diprivan®: 1683 ± 134.2
Diprivan® w/15 ml kg⁻¹ Intralipid®: 1030 ± 201.8

*slopes are significantly different (p = 0.014)
Slopes:

B8: 1217 ± 282.7
B8 w/15 ml kg⁻¹ Intralipid®: 602.2 ± 97.13

*slopes are significantly different (p = 0.046)
FIG. 10

- 15 mg/kg B8
- 15 mg/kg Diprivan

Graph showing RORR (s) vs. mL/kg Intralipid.
FLUOROPOLYMER EMULSIONS WITH PERHALOGENATED STABILIZER FOR THE DELIVERY OF HYDROPHOBIC DRUGS

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a U.S. National Stage Application filed under 35 U.S.C. § 371 of International Application No. PCT/US2015/027535, filed Apr. 24, 2015, which claims the benefit of U.S. Provisional Application No. 61/984,639, filed Apr. 25, 2014. All of these applications are hereby incorporated by reference in their entirety.

STATEMENT REGARDING FEDERALLY SPONSORED RESEARCH OR DEVELOPMENT

Not applicable.

BACKGROUND

Administration of hydrophobic drugs presents practical challenges due to the limited water solubility of this class of pharmaceuticals. Accordingly, a primary focus of drug delivery research is development of effective approaches for the formulation and controlled delivery for this class of important pharmaceutical agents. Nanoemulsions are a particularly promising delivery vehicle for these applications given their intrinsic stability and potential to access useful pharmacokinetic properties for drug administration, absorption and targeting.

Nanoemulsions are composed of nanoscale droplets of one immiscible liquid dispersed within another. In the context of many pharmaceutical applications, for example, the dispersed droplet phase of a nanoemulsion provides a central oil core, stably dispersed in an aqueous phase, that can act as an effective reservoir for hydrophobic drugs. Nanoemulsions for delivery applications often incorporate one or more surfactants and/or stabilizers to facilitate stabilization and improve drug solubilization of the dispersed phase. As nonequilibrium systems, preparation of a nanoemulsion typically involves an input of energy, for example, using a microfluidiser, high pressure homogeniser or ultrasonicator.

Typical droplet sizes for nanoemulsions for the delivery of pharmaceuticals are in the range of about 20-500 nm. The small droplet size characteristic of nanoemulsions provides benefits supporting their use as vehicles for pharmaceutical delivery. First, the small droplet size and lower surface tension between dispersed and aqueous phases decrease the rates of droplet agglomeration and precipitation processes so as to substantially limit the potential for phase separation via sedimentation, flocculation, coalescence and creaming. As a result, nanoemulsions are typically more kinetically stable than other types of emulsions. Second, the nanosized dimensions of the droplets allow for effective in vivo administration, for example via drug absorption from the gastrointestinal tract or penetration of the skin barrier. Third, the large interfacial area provided by the small size of the dispersed droplets allows for the potential to effectively control drug release over a clinical useful range. Accordingly, nanoemulsions have significant potential for providing rapid, sustained or targeted delivery and release of hydrophobic drugs.

While emulsions have long been used for topical administration, recent research has been directed to development of emulsion-based delivery systems effective for parenteral, inhalation and oral delivery. Phospholipid-stabilized soybean oil emulsions were the first approved intravenous emulsion and have been used clinically as i.v. nutritional supplements for over 40 years. More recently, however, emulsions have been developed and employed widely in the clinic for the delivery of certain hydrophobic drugs, such as anesthetics, anti-inflammatory and analgesic drugs, and also as blood substitutes.

Commercial propofol (i.e., Diprivan), for example, consists of an Intralipid® emulsion of the active agent 2,6-disopropylphenol. The lipid emulsion-based formulation of propofol is used extensively for anesthesiology practices for inducing and maintaining general anesthesia. In addition, this emulsion-based formulation of propofol is used for procedural sedation and sedation in intensive care settings. Current lipid emulsion-based formulations of propofol are susceptible to problems relating to the ability of their lipid component (e.g. soybean oil) to support bacterial and fungal growth. To address the risk of contamination, for example, tubing and open vials of propofol must be replaced every twelve hours for many clinical applications. In addition, infusion at high rates or as large bolus can result in lipid intolerance, which may contribute to propofol infusion syndrome, a rare but serious complication that further limits use of lipid-based emulsions of propofol in intensive care settings.

It will be appreciated from the foregoing that emulsion-based delivery systems for the formulation and administration of hydrophobic drugs are needed. Systems and formulations are needed that are capable of providing stable formulation of hydrophobic drugs exhibiting sparing solubility in aqueous solutions, particularly, in concentrations supporting a range of important clinical applications. Systems and formulations are needed exhibiting a high degree of biocompatibility, low toxicity and pharmacokinetic properties supporting controlled delivery and targeting of hydrophobic drugs.

SUMMARY OF THE INVENTION

The present invention provides therapeutic formulations, including therapeutic nanoemulsions, and related methods for the in vivo delivery of hydrophobic compounds, including an important class of hydrophobic anesthetics. Formulations and methods of the invention include semifluorinated block copolymers and perhalogenated fluorous compounds, such as perfluoroocetyl bromide or perfluorodecalin, capable of forming a stable nanoemulsion without the need for conventional lipid components that support bacterial and/or fungal growth (e.g., soybean oil and similar lipids). In certain embodiments, emulsion-based formulations are provided that are capable of formulating, delivering and releasing amounts of hydrophobic drugs effective for a range of clinical applications, including inducing and maintaining anesthesia in patients. In certain embodiments, emulsion-based formulations are provided that are capable of supporting controlled release, for example, over a range of rates useful for clinical applications including rapid and sustained release.

In certain embodiments, nanoemulsion formulations of the present invention include linear semifluorinated block copolymers and perhalogenated fluorous compounds having compositions resulting in enhanced stability with respect to droplet size by decreasing the rate of Ostwald ripening, coagulation and/or phase separation processes. Therapeutic formulations of the present invention also provide a high degree of versatility, as the amount and composition of the semifluorinated block copolymer component (e.g., length and composition of the hydrophilic block, length and com-
position of the fluorophilic block, length and composition of the hydrophobic block, etc.) and the amount and chemical composition of the perhalogenated fluoruous compounds may be selectively adjusted to: (i) enhance stability under delivery conditions, (ii) optimize the kinetics of release of a hydrophobic compound for a specific application (e.g., provide faster or slower release rates), and (iii) enhance the overall formulation stability of therapeutic nanoemulsions under storage conditions (e.g., increase useful shelf life).

In an embodiment, the present formulations comprise linear semi-fluorinated block copolymers having hydrophilic, hydrophobic and fluorophilic blocks, and optionally a stabilizing additive, such as a perhalogenated fluoruous compound, capable of generating an emulsion of a clinically effective amount of a hydrophobic compound, such as propofol, dispersed in an aqueous solution. Therapeutic formulations of the present invention include nanoemulsions comprising submicron droplets of a hydrophobic compound dispersed in a continuous phase comprising an aqueous solution, such as an aqueous solution isotonic to blood plasma. In some embodiments, droplets of the hydrophobic compound of the emulsion are stabilized by the formation of supramolecular structures of self-assembled semi-fluorinated block copolymer surfactants that reduce the interfacial tension of the hydrophobic compound at the droplet interface with the continuous aqueous phase. In some embodiments, for example, surfactant comprising linear semi-fluorinated block copolymers having a hydrophilic block, hydrophobic block and a fluorophilic block self-assemble upon emulsification to form supramolecular structures dispersed in an aqueous continuous phase, thereby encapsulating and stabilizing significant quantities of the hydrophobic compound component in a hydrophobic intermediate shell. For example, the hydrophobic block of the semifluorinated block copolymers may form an intermediate shell of the supramolecular structure, thereby functioning as a molecular recognition element for the hydrophobic compound. Optionally, the dispersed phase droplets of hydrophobic compound may also have a stabilizing additive component for providing useful chemical and physical properties.

In an aspect, the present invention provides emulsion-based formulations, such as nanoemulsions. For example, in one embodiment, an emulsion of the invention is useful for delivery of a therapeutic agent comprising a hydrophobic drug. Emulsions of this aspect are beneficial, for example, for delivering therapeutic agents comprising a hydrophobic compound to a patient or subject, such as a therapeutic agent which is insoluble or only sparingly soluble in aqueous solution. For example, in some embodiments, hydrophobic therapeutic agents which are soluble in aqueous solutions at concentrations or dosages less than a useful therapeutic amount benefit from the emulsions of the invention, which provide for the ability to deliver a therapeutic or effective amount of the therapeutic agent to a patient or subject. In some embodiments, for example, the nanoemulsions of the invention are useful for formulation and administration of hydrophobic anesthetic agents, such as propofol.

In an aspect, an emulsion of the invention comprises: an aqueous solution, semi-fluorinated block copolymers, a therapeutic agent comprising a hydrophobic compound and a perhalogenated fluoruous compound. In embodiments, for example, each of the semi-fluorinated block copolymers independently comprises a hydrophilic block, a hydrophobic block and a fluorophilic block, such as where the hydrophobic block of each of the semi-fluorinated block copolymers is provided between the fluorophilic block and the hydrophilic block. In exemplary embodiments, for example, the emulsion comprises a continuous phase and a dispersed phase, such as where the continuous phase comprises the aqueous solution and the dispersed phase comprises the semi-fluorinated block copolymers, the therapeutic agent and the perhalogenated fluoruous compound.

In an embodiment of this aspect, the emulsion is a nanoemulsion, for example, characterized by a dispersed phase comprising droplets having cross sectional dimensions selected from the range of 20 nm to 1 micron, and optionally selected from the range of 100 nm to 1 micron. In an embodiment, the dispersed phase droplets comprise a hydrophobic therapeutic agent, the perhalogenated fluoruous compound and optionally the semi-fluorinated block copolymers, wherein said droplets have an average diameter less than or equal to 1000 nanometers, preferably for some applications an average diameter less than or equal to 500 nanometers, and more preferably for some applications an average diameter less than or equal to 300 nanometers. Optionally, the therapeutic formulation of this aspect of the present invention is capable of delivery to a patient via parenteral administration, such as via intravenous injection.

Emulsions of the invention for certain applications, optionally exclude certain substances or mixtures of substances from either or both the dispersed phase and the aqueous phase. Emulsions of the invention optionally include certain substances or mixtures in either or both the dispersed phase and the aqueous phase. For example, in some embodiments, certain substances or mixtures are either explicitly excluded from or included in the emulsion in order to control the physical properties, emulsion ripening rate, emulsion stability, composition, toxicity, biocompatibility, therapeutic effectiveness, therapeutic agent delivery or release rate, immune or other physiological response or any combination of these. In various embodiments, for example, an emulsion does not contain a vegetable oil component, such as a soybean oil component. In certain embodiments, for example, an emulsion does not support bacterial growth. In some embodiments, for example, an emulsion does not contain a phospholipid component, such as an egg phospholipid component.

In embodiments, the composition and relative amounts of the components of the emulsions are selected so as to achieve a desired solubilization amount of one or more hydrophobic therapeutic agents, such as a clinically or therapeutically effective amount. In embodiments, the composition and relative amounts of the components of the emulsions are selected so as to achieve a desired or controlled release rate, release timing or targeted delivery of one or more hydrophobic therapeutic agents.

In embodiments, emulsions of the invention comprise semi-fluorinated block copolymers. The structure, composition, size or concentration of the semi-fluorinated block copolymers and polymer block components thereof are optionally selected so as to provide certain properties to the emulsion, such as physical properties, emulsion ripening rate, emulsion stability, therapeutic agent solubility, composition, toxicity, biocompatibility, therapeutic effectiveness, therapeutic agent delivery rate or release rate, immune or other physiological response or any combination of these. In an embodiment, the hydrophilic block and fluorophilic block as each independently polymer terminating blocks, for example, wherein the hydrophobic block is an intermediate block provided directly or indirectly between the hydrophilic block and fluorophilic block.

In embodiments, for example, the semi-fluorinated block copolymers have a concentration selected from the range of
1 mg mL\(^{-1}\) to 50 mg mL\(^{-1}\), optionally for some applications selected from the range of 5 mg mL\(^{-1}\) to 50 mg mL\(^{-1}\). In some embodiments, the semi-fluorinated block copolymers have a concentration selected from the range of 10 to 50 mg mL\(^{-1}\). In embodiments, for example, each of the semi-fluorinated block copolymers independently has a molecular weight selected from the range 100 Da to 20,000 Da, and optionally for some applications 1100 Da to 14,000 Da.

In certain embodiments, the structure, composition or size of the hydrophilic block of the semi-fluorinated block copolymers are selected so as to make stable emulsion-based formulations from a wide range of hydrophobic therapeutic agents, such as hydrophobic anesthetics. In exemplary embodiments, the hydrophilic block of each of the semi-fluorinated block copolymers is a polymer terminating group. In embodiments, the hydrophilic block is selected from the group consisting of a poly(oxygenated) polymer block, a polysaccharide block and a chitosan derivative block. In an embodiment, the hydrophilic block is a poly(oxygenated) block, such as a poly(ethylene glycol) block. In exemplary embodiments, the hydrophilic block is a poly(ethylene glycol) block, for example, having a molecular weight selected from the range of 500 g mol\(^{-1}\) to 20,000 g mol\(^{-1}\), optionally for some applications selected from the range of 1000 g mol\(^{-1}\) to 20,000 g mol\(^{-1}\), optionally for some applications selected from the range of 1000 g mol\(^{-1}\) to 15,000 g mol\(^{-1}\), and optionally for some applications selected from the range of 1000 g mol\(^{-1}\) to 10,000 g mol\(^{-1}\).

In some embodiments, selection of the size/molecular weight of the poly(ethylene glycol) block establishes the release rate of a hydrophobic therapeutic agent and/or stability of the nanoemulsion with respect to ripening, coagulation and phase separation processes. In some embodiments, the hydrophilic block is directly linked to the hydrophobic block.

In certain embodiments, the structure, composition or size of the fluorophilic block of the semi-fluorinated block copolymers are selected so as to make stable emulsion-based formulations from a wide range of hydrophobic therapeutic agents, such as hydrophobic anesthetics. In exemplary embodiments, the hydrophobic block is a polymer terminating group. In embodiments, the hydrophobic block is selected from the group consisting of a poly(oxygenated) polymer block, a poly(ester) block and poly(lactic-co-glycolic acid). In some embodiments, the hydrophobic block is an unsubstituted \(\text{C}_n\text{C}_{20}\) alkyne group, optionally an unsubstituted \(\text{C}_n\text{C}_{10}\) alkene group. In some embodiments, the hydrophobic block is a fluorocarbon moiety having between 3 to 50 carbon-fluorine bonds.

In certain embodiments, the structure, composition or size of the fluorophilic block of the semi-fluorinated block copolymers independently has the formula (FX1):

\[
\begin{align*}
\text{A} & \rightarrow L_1^{\pm m} B \rightarrow L_2^{\pm n} D;
\end{align*}
\]

where A is the hydrophilic block, B is the hydrophobic block and D is the fluorophilic block; where \(L_1\) and \(L_2\) are each independently a linking group; and where \(m = 0\) or 1 and \(n = 0\) or 1. For embodiments where \(m = 0\), \(L_1\) is not present and \(A\) and \(B\) are directly bonded to one another. For embodiments where \(n = 0\), \(L_2\) is not present and \(B\) and \(D\) are directly bonded to one another. In some embodiments, the semi-fluorinated block copolymers independently have the formula (FX1), wherein \(m = 0\). In some embodiments, the semi-fluorinated block copolymers have the formula (FX1), wherein \(n = 0\).

In certain embodiments, A is \(-(\text{CH}_2\text{CH}_2\text{O})_q\), where \(q\) is an integer selected from the range of 10 to 300, and optionally for some applications 10 to 300, and optionally for some applications 10 to 100 and optionally for some applications 20 to 50. In certain embodiments, A is \(-(\text{CH}_2)_o\), wherein \(o\) is an integer selected from the range of 5 to 30, and optionally for some applications 5 to 20, and optionally for some applications 5 to 15.

In certain embodiments, D is \(-(\text{CF}_2)_p\), where \(p\) is an integer selected from the range of 5 to 30, and optionally for some applications 5 to 20, and optionally for some applications 5 to 15. In certain embodiments, D is \(-(\text{CF}_2)_p\), where \(p\) is an integer selected from the range of 5 to 30, and optionally for some applications 5 to 20, and optionally for some applications 5 to 15.
In a specific embodiment, each of the semi-fluorinated block copolymers independently has the formula (FX2):

\[ \text{(FX2)} \]

\[ R^1 \left\{ \begin{array}{c} \bigwedge^q \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \end{array} \right\} \]

where \( q \) is an integer selected from the range of 10 to 300, \( o \) is an integer selected from the range of 5 to 20, and \( p \) is an integer selected from the range of 3 to 15; where \( R^2 \) is hydrogen, methyl, \( C_1-C_{10} \) alkyl, \( C_5-C_{10} \) cycloalkyl, \( C_6-C_{10} \) aryl, \( C_3-C_{10} \) heteroaryl, \( C_1-C_{10} \) alkoxy or \( C_3-C_{10} \) acyl; where \( L^1 \) is hydrogen, halo or \( C_1-C_3 \) alkyl; where each of \( L^1 \) and \( L^2 \) is independently \( -(\text{CH}_2)_n-\); \( -(\text{CH}_2)_n\text{S}(\text{CH}_2)_m-\); \( -(\text{CH}_2)_n\text{NR}^1(\text{CH}_2)_m-\); \( -(\text{CH}_2)_n\text{CONR}^2(\text{CH}_2)_m-\); \( -(\text{CH}_2)_n\text{CONR}^3(\text{CH}_2)_m-\); \( -(\text{CH}_2)_n\text{NR}^1\text{CO}(\text{CH}_2)_m-\); \( -(\text{CH}_2)_n\text{NR}^3\text{CONR}^2(\text{CH}_2)_m-\); or \( -(\text{CH}_2)_n\text{NR}^1\text{CO}(\text{CH}_2)_m-\) where each of \( R^1-R^7 \) is independently hydrogen, methyl, or \( C_1-C_2 \) alkyl; and where each of \( e \) and \( f \) is independently an integer selected from the range of 0 to 5; and where \( m \) is 0 or 1 and \( n \) is 0 or 1. In a specific embodiment, the semi-fluorinated block copolymers independently has the formula (FX2) and a halogen is selected from the group consisting of \( F \), \( Cl \) and \( Br \). In a specific embodiment, when \( e \) is 0, the \( (\text{CH}_2)_e \) group is not present and moieties adjacent to the \( (\text{CH}_2)_e \) group in the above described structures for \( L^1 \) and \( L^2 \) are directly bonded to one another. In a specific embodiment, when \( f \) is 0, the \( (\text{CH}_2)_f \) group is not present and moieties adjacent to the \( (\text{CH}_2)_f \) group in the above described structures for \( L^1 \) and \( L^2 \) are directly bonded to one another. In some embodiments, the semi-fluorinated block copolymers independently has the formula (FX2), wherein \( m \) is 0. In some embodiments, the semi-fluorinated block copolymers independently has the formula (FX7), wherein \( n \) is 0.

In some embodiments, the semi-fluorinated block copolymers independently has the formula (FX2), wherein \( q \) is an integer selected from the range of 10 to 200, and optionally for some applications 10 to 100 and optionally for some applications 10 to 50. In some embodiments, the semi-fluorinated block copolymers independently has the formula (FX2), wherein \( o \) is an integer selected from the range of 5 to 16, and optionally for some applications 5 to 16. In some embodiments, the semi-fluorinated block copolymers independently has the formula (FX2), wherein \( p \) is an integer selected from the range of 5 to 15, and optionally for some applications 8 to 15. In some embodiments, the semi-fluorinated block copolymers independently has the formula (FX2), wherein \( R^1 \) is hydrogen, \( C_1-C_{10} \) alkyl, and optionally methyl or methoxy. In some embodiments, the semi-fluorinated block copolymers independently has the formula (FX2), wherein \( R^2 \) is hydrogen or halo, optionally \( F \). In some embodiments, the semi-fluorinated block copolymers independently has the formula (FX2), wherein each of \( R^1-R^7 \) is independently hydrogen or \( C_1-C_4 \) alkyl, optionally methyl.

In a specific embodiment, \( L^1 \) is \( -\bigwedge^q \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \). In a specific embodiment, \( L^2 \) is \( -\bigwedge^o \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \). In a specific embodiment, each of the semi-fluorinated block copolymers independently has the formula (FX3A) or (FX3B):

\[ \text{(FX3A)} \]

\[ R^1 \left\{ \begin{array}{c} \bigwedge^q \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \end{array} \right\} \]

\[ \bigwedge^o \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

\[ \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

\[ \bigwedge^o \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

In a specific embodiment, \( R^1 \) is \( \bigwedge^q \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \). In a specific embodiment, \( R^2 \) is \( \bigwedge^o \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \). In a specific embodiment, each of the semi-fluorinated block copolymers independently has the formula (FX4) or (FX4B):

\[ \text{(FX4B)} \]

\[ R^1 \left\{ \begin{array}{c} \bigwedge^q \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \end{array} \right\} \]

\[ \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

\[ \bigwedge^o \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

\[ \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

\[ \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

In a specific embodiment, \( R^1 \) is \( \bigwedge^q \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \). In a specific embodiment, \( R^2 \) is \( \bigwedge^o \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \). In a specific embodiment, each of the semi-fluorinated block copolymers independently has the formula (FX5A) or (FX5B):

\[ \text{(FX5A)} \]

\[ R^1 \left\{ \begin{array}{c} \bigwedge^q \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \end{array} \right\} \]

\[ \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

\[ \bigwedge^o \bigl( \text{CH}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

\[ \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

\[ \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \bigwedge^p \bigl( \text{CF}_2 \bigl) \]

In certain embodiments, the structure, composition, size or concentration of the perhalogenated fluorocarbons used in the invention is selected so as to make stable emulsion-based formulations from a wide range of hydrophobic therapeutic agents, such as hydrophobic anesthetics. In embodiments, the structure, composition, size or concentration of the perhalogenated fluorocarbon compound are selected so as to provide certain properties to the emulsion, such as physical properties, emulsion ripening rate, emulsion stability, therapeutic agent solubility, composition, toxicity, biocompatibility, therapeutic effectiveness, therapeutic agent delivery rate or release rate, immune or other physiological response or any combination of these. For example, in one embodiment, the perhalogenated fluorocarbon is an emulsion stabilizing additive. In one embodiment, for example, the perhalogenated fluorocarbon is 5% to 30% by volume of the emulsion, optionally for some applications 5% to 20% by volume, and optionally for some applications 5% to 10% by volume.

Selection of the perhalogenated fluorocarbon compound, such as a perhalogenated fluorocarbon compound, having specific and well defined physical and chemical properties is also important in the present invention for providing therapeutic formulations providing enhanced delivery performance and stability, and for accessing therapeutic emulsions having clinically effective concentrations of hydrophobic compounds. In some embodiments, for example, the perhalogenated fluorocarbon compound is provided that comprises a component of the dispersed droplet phase that controls the release rate of the hydrophobic compound from the droplets, thereby lowering the rate of droplet ripening processes such as Ostwald ripening. The perhalogenated fluorocarbon of this aspect is useful for providing therapeutic emulsions, including nanoemulsions, exhibiting stable drop-
reagents are that no toxicity, carcinogenic, mutagenic, tera-
gen effects, or immunological reactions, have been
ported for many fluorocarbons when provided in a suffi-
ciently pure form and chosen within an appropriate molecu-
lar weight range.

A variety of perhalogenated fluorous compounds are use-
ul with the emulsions of the invention. In one embodi-
ment, the perhalogenated fluorous compound has 12 to 25
carbon-fluorine bonds, optionally for some applications 15
to 20 carbon-fluorine bonds. In an exemplary embodiment,
the perhalogenated fluorous compound is a substituted or
unsubstituted fluorocarbon having a length of 4 to 20
carbons, and optionally for some applications 5 to 15
carbons, and optionally for some applications 5 to 10
carbons. In embodiments, the perhalogenated fluorous com-
 pound comprises a perfluorocarbon. In embodiments, the
perhalogenated fluorous compound comprises a perfluoro-
carbon in which one or more fluorine atoms are substituted
with Cl, Br or I, optionally in which one or more fluorine
atoms are substituted with Cl or Br. In various embodi-
ments, the substituted or unsubstituted fluorocarbon is linear,
branched or cyclic. In embodiments, the substituted or
unsubstituted fluorocarbon is a substituted or unsubstituted
C₆H₅F₉ fluoralkane, and optionally for some applications
C₅H₅F₉ fluoralkane.

In embodiments, for example, the perhalogenated fluoro-
s compound has a solubility in water less than or equal
to 20 nanomolar. In embodiments, for example, the perhal-
genated fluorous compound has a molecular weight
selected over the range of 460 amu to 920 amu. In exem-
plary embodiments, the perhalogenated fluorous compound
is selected from the group consisting of: a perfluorocarbo-

A variety of specific perhalogenated fluorous compounds
are useful with the emulsions of the invention. In specific
embodiments, for example, the perhalogenated fluorous
compound is selected from the group consisting of perflu-
oroctyl bromide, perfluorononyl bromide, perfluorodecyl
bromide, perfluorodecafluorooctane, bis-perfluoro-
butyl ethylene and perfluoro(methyldecalin). In embodi-
ments, the perhalogenated fluorous compound is
perfluoroctyl bromide or perfluorodecalin. In embodi-
ments, the perhalogenated fluorous compound is perflu-
oroctyl bromide.

Optionally, emulsions of the invention further comprise
one or more additional perhalogenated fluorous compo-
dounds including, for example, any of the perhalogenated fluorous
compounds disclosed herein. Optionally, emulsions of the
invention further comprise one or more additional fluorocar-
bon stabilizing additives including, for example, any of
the fluorocarbon stabilizing additives herein. Emulsions
of the invention include formulations comprising two or more
of any of the perhalogenated fluorous compounds disclosed
herein, for example, the combination of perfluoroctyl bro-
mide and perfluorodecalin.

A variety of therapeutic agents are useful with the emul-
sions of the invention. In certain embodiments, the structure,
composition, size or concentration of the therapeutic agent
is selected so as to make a stable emulsion-based formula-
tion. In embodiments, the structure, composition, size or
concentration of the therapeutic agent are selected so as
to provide certain properties to the emulsion, such as physical
properties, emulsion ripening rate, emulsion stability, ther-
apeutic agent solubility, composition, toxicity, biocompatibil-
ity, therapeutic effectiveness, therapeutic agent delivery rate or release rate, immune or other physiological response or any combination of these. In an embodiment, for example, the therapeutic agent has a concentration of at least 0.2 mg mL⁻¹ in the emulsion, and optionally for some embodiments at least 1 mg mL⁻¹. In an embodiment, the therapeutic agent has a concentration selected from the range of 0.2 mg mL⁻¹ to 30 mg mL⁻¹ in the emulsion.

In certain embodiments, the therapeutic agent is a hydrophobic compound. Use of hydrophobic therapeutic agents is beneficial as a variety of hydrophobic therapeutic agents exhibit reduced toxicity, increased therapeutic effectiveness or smaller required therapeutic dosages as compared to some non-hydrophobic therapeutic agents. In addition, therapeutic agents for a desired clinical application may only be available as a hydrophobic compound. In embodiments, emulsions of the invention are, thus, particularly useful for providing a therapeutically deliverable quantity of a hydrophobic therapeutic agent in order to achieve a desired clinical outcome, such as anesthesia. In a specific embodiment, the hydrophobic compound has a concentration of 0.2 to 50 mg mL⁻¹, optionally for some applications a concentration of 1 to 50 mg mL⁻¹. In an embodiment, for example, the hydrophobic compound is characterized by a solubility in water of equal to or less than 5 mM, optionally for some applications equal to or less than 1 mM and optionally equal to or less than 0.7 mM. For reference, the solubility of propofol in water is 0.124 mg/ml corresponding to 0.696 mM.

In a specific embodiment, the hydrophobic compound is noncovalently associated with the hydrophobic block, the fluorophilic block or both the hydrophobic block and the fluorophilic block of the semi-fluorinated block copolymers. For example, in embodiments, the hydrophobic compound is dissolved or solvated by a hydrophobic block, a fluorophilic block or both, such that the hydrophobic compound is suspended or otherwise deliverable by an emulsion of the invention.

A variety of hydrophobic compounds are useful with the emulsions of the invention. In a specific embodiment, the hydrophobic compound is a hydrophobic drug. In a specific embodiment, the hydrophobic compound is an anesthetic drug. In embodiments, the hydrophobic compound is a substituted or unsubstituted aromatic compound or a substituted or unsubstituted heteroaromatic compound. In a specific embodiment, for example, the hydrophobic compound is a neurosteroid drug. In exemplary embodiments, the anesthetic drug is propofol or alfaxalone. Optionally, the anesthetic drug has a concentration of 10 to 50 mg mL⁻¹; and the semi-fluorinated block copolymers comprise the hydrophobic compound at a concentration of 0.2 to 50 mg mL⁻¹; and the semi-fluorinated block copolymers at a concentration selected from the range of 10 to 50 mg mL⁻¹. Exemplary emulsion embodiments are useful for administration to a patient in need thereof via intravenous injection.

Emulsions of embodiments of the invention are stable and possess a shelf life such that the emulsions do not quickly settle into two or more phases and thus are suitable for administration to a patient or subject at a time period after the emulsion is prepared or manufactured, such as a time period greater than 1 day or greater than 1 month. In an exemplary embodiment, the droplets do not undergo an appreciable change in size over a period of 1 day to 4 weeks. In embodiments, for example, an appreciable change in size is a change that is greater than or equal to a 10% increase.

For certain embodiments, an emulsion of the invention comprises a nanoeulsion. For example, in some embodiments, the emulsion comprises droplets having an average diameter selected from the range of 1 nm to 500 nm. For example, in some embodiments, the emulsion comprises droplets having an average diameter less than 1000 nm. In some embodiments, the emulsion comprises droplets having an average diameter less than 400 nm. For some embodiments, the emulsion does not comprise micelles. For some embodiments, the emulsion does not comprise vesicles. In certain embodiments, the emulsion is not a microemulsion. For some embodiments, the emulsion comprises a supramolecular structure. For other embodiments, the emulsion does not comprise a supramolecular structure.

In another aspect, the present invention provides methods. A method of this aspect comprises a method of delivering a therapeutic agent to a patient in need thereof. In an embodiment, such a method comprises, for example, the steps of: providing an emulsion comprising: an aqueous solution; semi-fluorinated block copolymers; a therapeutic agent comprising a hydrophobic compound; and a perhalogenated fluorous compound; wherein each of the semi-fluorinated block copolymers independently comprises a hydrophilic block, a hydrophobic block and a fluorophilic block; wherein the hydrophobic block of each of the semi-fluori-
nated block copolymers is provided between the fluorophilic block and the hydrophilic block; wherein the emulsion comprises a continuous phase and a dispersed phase, wherein the continuous phase comprises the aqueous solution and the dispersed phase comprises the semi-fluorinated block copolymers, the therapeutic agent and the perhalogenated fluorous compound; and administering the emulsion to the patient, wherein the therapeutic agent is released from the emulsion, thereby delivering the therapeutic agent to the patient in need thereof.

In exemplary embodiments, an emulsion administered to a patient comprises any of the emulsions described previously herein. In a specific embodiment, an emulsion administered to a patient is a nanoemulsion. In a specific embodiment, the hydrophobic compound administered to a patient is a hydrophobic drug, such as an anesthetic drug, for example, propofol.

In exemplary embodiments of methods of this aspect, the step of administering the emulsion provides for controlled release of the hydrophobic drug from the emulsion. Optionally, the step of administering the emulsion is carried out via intravenous injection. In a specific embodiment, a volume of the emulsion less than or equal to 500 mL is administered to the patient. In exemplary embodiments, a volume of the emulsion selected from the range 0.1 mL to 500 mL is administered to the patient. In a specific embodiment, the emulsion is delivered to the patient at a rate less than or equal to 100 mL per minute. In exemplary embodiments, the emulsion is delivered to the patient at a rate selected from the range of 0.01 to 10 mL per minute.

In a further aspect, provided are methods of making emulsions. In exemplary embodiments, the emulsion is a nanoemulsion. An exemplary method of this aspect comprises the steps of: providing a therapeutic formulation comprising: an aqueous solution; semi-fluorinated block copolymers; wherein each of the semi-fluorinated block copolymers independently comprises a hydrophilic block, a hydrophobic block and a fluorophilic block; wherein the hydrophilic block of each of the semi-fluorinated block copolymers is provided between the fluorophilic block and the hydrophobic block; a therapeutic agent comprising a hydrophobic compound; and a perhalogenated fluorous compound; and emulsifying the therapeutic formulation, thereby making an emulsion comprising a continuous phase and a dispersed phase, wherein the continuous phase comprises the aqueous solution and the dispersed phase comprises the semi-fluorinated block copolymers, the therapeutic agent and the perhalogenated fluorous compound.

In certain embodiments of methods of this aspect, the step of emulsifying the therapeutic formulation comprises the steps of: adding the hydrophobic compound and the perhalogenated fluorous compound to the aqueous solution having the semi-fluorinated block copolymers therein, thereby generating a mixture; and homogenizing the mixture, thereby generating the emulsion. In exemplary embodiments, methods of this aspect further comprise a step of lowering a temperature of the mixture during the step of homogenizing the mixture. In embodiments, for example, the step of homogenizing the mixture is carried out using a lower energy mixer, a microfluidizer or both. Low-energy mixers are known in the art, such as described in AlChE J., 57:27-39. doi: 10.1002/aic.12253.

Without wishing to be bound by any particular theory, there may be discussion herein of beliefs or understandings of underlying principles relating to the devices and methods disclosed herein. It is recognized that regardless of the ultimate correctness of any mechanistic explanation or hypothesis, an embodiment of the invention can nonetheless be operative and useful.

**BRIEF DESCRIPTION OF THE DRAWINGS**

FIG. 1 provides a schematic illustration of the formation of dispersed phase droplets in an emulsion.

FIG. 2 provides a plot showing the mean droplet diameter (nm) for the emulsions corresponding to Formulations 1, 2 and 3 evaluated as a function of time (days).

FIG. 3 provides plots of time to Loss of Righting Reflex (LORR) (s) as a function of dose (mg/kg).

FIG. 4 provides plots of time to Time to Return of Righting Reflex (s) as a function of dose (mg/kg).

FIG. 5 provides a plot showing the average particle size (nm) for the emulsions corresponding to Formulations B8 and L3 were evaluated as a function of time (days).

FIG. 6 provides a plot showing the average particle size (nm) for the emulsions corresponding to formulations M1H10FS9FPOE, M5diH10, and Lipoid E80 were evaluated as a function of time (days).

FIG. 7 provides plots of time to Time to Return of Righting Reflex (s) as a function of the logarithm of the dose (mg/kg).

FIG. 8 provides plots of time to Time to Return of Righting Reflex (s) as a function of the logarithm of the dose (mg/kg).

FIG. 9 provides plots of time to Time to Return of Righting Reflex (s) as a function of the logarithm of the dose (mg/kg).

FIG. 10 provides plots of time to Time to Return of Righting Reflex (s) vs Intralipid® dose (mL/kg).
more cycloalkylene groups. Cycloalkyl groups in some
compositions of the invention, and as will be understood by one of
thereof.

As used herein, the term “group” may refer to a functional
group of a chemical compound. Groups of the present
compounds refer to an atom or a collection of atoms that are
a part of the compound. Groups of the present invention may
be attached to other atoms of the compound via one or more
covalent bonds. Groups may also be characterized with
respect to their valence state. The present invention includes
groups characterized as monovalent, divalent, trivalent, etc.
valence states.

As used herein, the term “substituted” refers to a com-

As is customary and well known in the art, hydrogen
atoms in formulas (FX1)-(FX5) are not always explicitly
shown, for example, hydrogen atoms bonded to the carbon
atoms of aromatic, heteroaromatic, and alicyclic rings are
not always explicitly shown in formulas (FX1)-(FX5). The
structures provided herein, for example in the context of the
description of formulas (FX1)-(FX5), are intended to con-
voy to one of reasonable skill in the art the chemical
composition of compounds of the methods and composi-
tions of the invention, and as will be understood by one of
skill in the art, the structures provided do not indicate the
specific positions of atoms and bond angles between atoms
of these compounds.

As used herein, the terms “alkylene” and “alkylene
group” are used synonymously and refer to a
divalent group derived from an alkyl group as defined herein. The invention
includes compounds having one or more alkylene groups.
Alkylene groups in some compounds function as attaching and/or spacer groups.
Compounds of the invention may have substituted and/or unsubstituted C₃-C₂₀ alkylene, C₁-C₁₀ alkylene and C₁-C₅ alkylene groups.

As used herein, the terms “cycloalkyl” and “cycloalkylene group” are used synonymously and refer to a
divalent group derived from a cycloalkyl group as defined herein. The invention includes compounds having one or more cycloalkylene groups. Cycloalkylene groups in some compounds function as attaching and/or spacer groups.
Compounds of the invention may have substituted and/or unsubstituted C₃-C₂₀ cycloalkylene, C₁-C₁₀ cycloalkylene and C₁-C₅ cycloalkylene groups.

As used herein, the terms “arylene” and “arylene group” are used synonymously and refer to a
divalent group derived from an aryl group as defined herein. The invention includes compounds having one or more arylene groups. Arylene groups in some compounds function as attaching and/or spacer groups.
Compounds of the invention may have substituted and/or unsubstituted C₃-C₂₀ arylene, C₁-C₁₀ arylene and C₁-C₅ arylene groups.

As used herein, the terms “heteroarylene” and “heteroarylene group” are used synonymously and refer to a
divalent group derived from a heteroaryl group as defined herein. The invention includes compounds having one or more heteroarylene groups. Heteroarylene groups in some compounds function as attaching and/or spacer groups.
Compounds of the invention may have substituted and/or unsubstituted C₃-C₂₀ heteroarylene, C₁-C₁₀ heteroarylene and C₁-C₅ heteroarylene groups.

As used herein, the terms “alkenylene” and “alkenylene group” are used synonymously and refer to a
divalent group derived from an alkenyl group as defined herein. The invention includes compounds having one or more alkenylene groups. Alkenylene groups in some compounds function as attaching and/or spacer groups.
Compounds of the invention may have substituted and/or unsubstituted C₃-C₃₀ alkenylene, C₁-C₁₀ alkenylene and C₁-C₅ alkenylene groups.

As used herein, the terms “halo” refers to a halogen group
such as a fluoro (−F), chloro (−Cl), bromo (−Br), iodo (−I) or astato (−At).

The term “heterocyclic” refers to ring structures contain-
ing at least one other kind of atom, in addition to carbon, in the ring. Examples of such heteroatoms include nitrogen, oxygen and sulfur. Heterocyclic rings include heterocyclic alicyclic rings and heterocyclic aromatic rings. Examples of heterocyclic rings include, but are not limited to, pyrroldinyl, piperidinyl, imidazolidinyl, tetrahydrofuranyl, tetrahydrothienyl, furyl, thi enyl, pyridyl, quinolyl, isoquinolyl, pyridazinyl, pyrazinyl, indolyl, imidazolyl, oxazolyl, thi azolyl, pyrazolyl, pyridinyl, benzoxadiazolyl, benzothiadiazolyl, triazolyl and tetrazolyl groups. Atoms of heterocyclic rings can be bonded to a wide range of other atoms and functional
groups, for example, provided as substituents.

The term “carbocyclic” refers to ring structures contain-
ing only carbon atoms in the ring. Carbon atoms of carbo-
cyclic rings can be bonded to a wide range of other atoms and functional
groups, for example, provided as substituents.

The term “allylic” refers to a ring, or plurality of fused rings, that is not an aromatic ring. Alicyclic rings include both carbocyclic and heterocyclic rings.

The term “aromatic” refers to a ring, or a plurality of fused rings, that includes at least one aromatic ring group.

The term “aliphatic” refers to a ring, or a plurality of fused rings, that includes at least one aromatic ring group.

The term “aromatic” refers to a ring, or a plurality of fused rings, that includes at least one aromatic ring group.

The term “aliphatic” refers to a ring, or a plurality of fused rings, that includes at least one aromatic ring group.
The term “fused ring” or “fused ring structure” refers to a plurality of alicyclic and/or aromatic rings provided in a fused ring configuration, such as fused rings that share at least two intra ring carbon atoms and/or heteroatoms.

As used herein, the term “alkoxy” refers to a substituent of the formula alkyl-O-alkyl.

As used herein, the term “polyhydroxyalkyl” refers to a substituent having from 2 to 12 carbon atoms and to from 2 to 5 hydroxyl groups, such as the 2,3-dihydroxypropyl, 2,3,4-tri hydroxybutyl or 2,3,4,5-tetrahydroxypentyl residue.

As used herein, the term “polyalkoxyalkyl” refers to a substituent of the formula alkyl-(alkoxy)n-alkoxy wherein n is an integer from 1 to 10, preferably 1 to 4, and more preferably for some embodiments 1 to 3.

Amino acids include glycine, alanine, valine, leucine, isoleucine, methionine, proline, phenylalanine, tryptophan, asparagine, glutamine, glycine, serine, threonine, serine, rhreonine, asparagine, glutamine, tyrosine, cysteine, lysine, arginine, histidine, aspartic acid and glutamic acid. As used herein, reference to “a side chain residue of a natural amino acid” specifically includes the side chains of the above-referenced amino acids.

Alkyl groups include straight-chain, branched and cyclic alkyl groups. Alkyl groups include those having from 1 to 30 carbon atoms. Alkyl groups include small alkyl groups having 1 to 3 carbon atoms. Alkyl groups include medium length alkyl groups having from 4-10 carbon atoms. Alkyl groups include long alkyl groups having more than 10 carbon atoms, particularly those having 10-30 carbon atoms. The term cycloalkyl specifically refers to an alkyl group having a ring structure such as ring structure comprising 3-30 carbon atoms, optionally 3-20 carbon atoms and optionally 2-10 carbon atoms, including an alkyl group having one or more rings. Cycloalkyl groups include those having a 3-, 4-, 5-, 6-, 7-, 8-, 9- or 10-member carbon ring(s) and particularly those having a 3-, 4-, 5-, 6-, or 7-member ring(s). The carbon rings in cycloalkyl groups can also carry alkyl groups. Cycloalkyl groups can include bicyclic and tricyclic alkyl groups. Alkyl groups are optionally substituted. Substituted alkyl groups include among others those which are substituted with alkyl or aryl groups, which groups in turn can be optionally substituted. Specific alkyl groups include ethyl, prop-1-enyl, prop-2-enyl, cyclopropyl, cyclopentyl, cyclohexyl, branched hexenyl, cyclohexenyl, all of which are optionally substituted. Alkyl groups include medium length alkyl groups having 3-10 carbon atoms, particularly those having 3-5 carbon atoms. Alkyl groups include long alkyl groups having from 12-20 carbon atoms, particularly those having 12-15 carbon atoms. Alkyl groups include long alkyl groups having more than 10 carbon atoms, particularly those having 10-30 carbon atoms.

Alkenyl groups include small alkenyl groups having 2 to 3 carbon atoms. Alkenyl groups include medium length alkenyl groups having from 4-10 carbon atoms. Alkenyl groups include long alkenyl groups having more than 10 carbon atoms, particularly those having 10-20 carbon atoms.

Alyl groups include those having from 1 to 30 carbon atoms. Alkenyl groups include small alkenyl groups having 2 to 3 carbon atoms. Alkenyl groups include medium length alkenyl groups having from 4-10 carbon atoms. Alkenyl groups include long alkenyl groups having more than 10 carbon atoms, particularly those having 10-20 carbon atoms.

Alkenyl groups include small alkenyl groups having 2 to 3 carbon atoms. Alkenyl groups include medium length alkenyl groups having from 4-10 carbon atoms. Alkenyl groups include long alkenyl groups having more than 10 carbon atoms, particularly those having 10-20 carbon atoms. Alkenyl groups include small alkenyl groups having 2 to 3 carbon atoms. Alkenyl groups include medium length alkenyl groups having from 4-10 carbon atoms. Alkenyl groups include long alkenyl groups having more than 10 carbon atoms, particularly those having 10-20 carbon atoms.
furan, dibenzofuran, carbazole, acridine, acridone, phenanthridine, thiophene, benzothiophene, dibenzothiophene, xanthene, xanthone, flavone, coumarin, azulene or anthracene. As used herein, a group corresponding to the groups listed above expressly includes an aromatic or heterocyclic aromatic group, including monovalent, divalent and polyvalent groups, of the aromatic and heterocyclic aromatic groups listed herein are provided in a covalently bonded configuration in the compounds of the invention at any suitable point of attachment. In embodiments, aryl groups contain between 5 and 30 carbon atoms. In embodiments, aryl groups contain one aromatic or heteroaromatic six-membered ring and one or more additional five- or six-membered aromatic or heteroaromatic ring. In embodiments, aryl groups contain between 5 and 18 carbon atoms in the rings. Aryl groups optionally have one or more aromatic rings or heterocyclic aromatic rings having one or more electron donating groups, electron withdrawing groups and/or targeting ligands provided as substituents. Arylalkyl groups are alkyl groups substituted with one or more aryl groups wherein the alkyl groups optionally carry additional substituents and the aryl groups are optionally substituted. Specific alkylaryl groups are phenyl-substituted alkyl groups, e.g., phenylmethyl groups. Alkylaryl groups are alternatively described as aryl groups substituted with one or more alkyl groups wherein the alkyl groups optionally carry additional substituents and the aryl groups are optionally substituted. Specific alkylaryl groups are alkyl-substituted phenyl groups such as methylphenyl. Substituted arylalkyl groups include fully halogenated or semihalogenated arylalkyl groups, such as arylalkyl groups having one or more alkyl and/or aryl groups having one or more hydrogens replaced with one or more fluorine atoms, chlorine atoms, bromine atoms and/or iodine atoms.

As to any of the groups described herein which contain one or more substituents, it is understood that such groups do not contain any substitution or substitution patterns which are sterically impractical and/or synthetically non-feasible. In addition, the compounds of this invention include all stereochemical isomers arising from the substitution of these compounds. Optional substitution of alkyl groups includes substitution with one or more alkyl groups, aryl groups or both, wherein the alkyl groups or aryl groups are optionally substituted. Optional substitution of alkyl groups includes substitution with one or more alkyl groups, aryl groups or both, wherein the alkyl groups or aryl groups are optionally substituted. Optional substitution of aryl groups includes substitution of the aryl ring with one or more alkyl groups, aryl groups or both, wherein the alkyl groups or aryl groups are optionally substituted. Optional substitution for any alkyl, aryl and aryl group includes substitution with one or more of the following substituents, among others:

- halogen, including fluorine, chlorine, bromine or iodine; pseudohalides, including —CN;
- COOR where R is a hydrogen or an alkyl group or an aryl group and more specifically where R is a methyl, ethyl, propyl, butyl, or phenyl group all of which groups are optionally substituted;
- COR where R is a hydrogen or an alkyl group or an aryl group and more specifically where R is a methyl, ethyl, propyl, butyl, or phenyl group all of which groups are optionally substituted;
- CON(R)₂ where each R, independently of each other R, is a hydrogen or an alkyl group or an aryl group and more specifically where R is a methyl, ethyl, propyl, butyl, or phenyl group all of which groups are optionally substituted; and R and R can form a ring which can contain one or more double bonds and can contain one or more additional carbon atoms; 
- OCON(R)₂ where each R, independently of each other R, is a hydrogen or an alkyl group or an aryl group and more specifically where R is a methyl, ethyl, propyl, butyl, phenyl or acetyl group, all of which are optionally substituted; and where R and R can form a ring which can contain one or more double bonds and can contain one or more additional carbon atoms;
- N(R)₂ where each R, independently of each other R, is a hydrogen, or an alkyl group, or an aryl group and more specifically where R is a methyl, ethyl, propyl, butyl, phenyl or acetyl group, all of which are optionally substituted; and where R and R can form a ring which can contain one or more double bonds and can contain one or more additional carbon atoms;
- SR, where R is hydrogen or an alkyl group or an aryl group and more specifically where R is hydrogen, methyl, ethyl, propyl, butyl, or phenyl group, which are optionally substituted;
- SO₂R, or —SOR where R is an alkyl group or an aryl group and more specifically where R is a methyl, ethyl, propyl, butyl, or phenyl group, all of which are optionally substituted;
- COOR where R is an alkyl group or an aryl group; and
- SO₃N(R)₂ where each R, independently of each other R, is a hydrogen, or an alkyl group, or an aryl group all of which are optionally substituted and wherein R and R can form a ring which can contain one or more double bonds and can contain one or more additional carbon atoms;
- OR where R is H, an alkyl group, an aryl group, or an acyl group all of which are optionally substituted. In a particular example R can be an acyl yielding
- OCOR* where R is a hydrogen or an alkyl group or an aryl group and more specifically where R is methyl, ethyl, propyl, butyl, or phenyl groups all of which groups are optionally substituted; and
- NO₂.

Specific substituted alkyl groups include haloalkyl groups, particularly trihalomethyl groups and specifically trifluoromethyl groups. Specific substituted aryl groups include mono-, di-, tri-, tetra- and pentahalo-substituted phenyl groups; mono-, di-, tri-, tetra-, penta-, hexa-, and hepta-halo-substituted naphthalene groups; 1- or 4-halo-substituted phenyl groups, 3- or 4-alkyl-substituted phenyl groups, 3- or 4-alkoxy-substituted phenyl groups, 3- or 4-alkoxy-substituted phenyl groups, 3- or 4-fluoro-substituted phenyl groups, particularly 2,4-difluorophenyl groups; fluorophenyl groups, particularly 3-fluorophenyl and 4-fluorophenyl groups; chlorophenyl groups, particularly 3-chlorophenyl and 4-chlorophenyl groups; methylphenyl groups, particularly 4-methylphenyl groups; and methoxyphenyl groups, particularly 4-methoxyphenyl groups.

As to any of the above groups which contain one or more substituents, it is understood that such groups do not contain any substitution or substitution patterns which are sterically impractical and/or synthetically non-feasible. In addition, the compounds of this invention include all stereochemical isomers arising from the substitution of these compounds. Pharmaceutically acceptable salts comprise pharmaceutically acceptable anions and/or cations. As used herein, the term “pharmaceutically acceptable salt” can refer to acid
addition salts or base addition salts of the compounds in the present disclosure. A pharmaceutically acceptable salt is any salt which retains at least a portion of the activity of the parent compound and does not impart significant deleterious or undesirable effect on a subject to whom it is administered and in the context in which it is administered. Pharmaceutically acceptable salts include metal complexes and salts of both inorganic and organic acids. Pharmaceutically acceptable salts include metal salts such as aluminum, calcium, iron, magnesium, manganese and complex salts. Pharmaceutically acceptable salts include, but are not limited to, acid salts such as acetic, aspartic, alkylsulfonic, arylsulfonic, axetil, benzensulfonyl, benzoic, bicarboxic, bisulfuric, bitartaric, butyric, calcium edetate, camsylic, carbonic, chloro- benzoic, -cilexetil, citric, edetic, edisyl, esyl, esyllic, formic, fumaric, gluceptic, gluconic, glutamic, glycolic, glycoylarsanilic, hexamic, hexylresorcinol, hydrobamic, hydrobromic, hydrochloric, hydroiodic, hydroxyphosphoric, isethionic, lactic, lactobionic, maleic, malic, malonic, mandelic, methansulfonic, methylhalritic, methylsulfuric, mucic, muconic, napsylic, nitrile, oxalic, p-nitromethanesulfonic, pamoic, pantothenic, phosphoric, monohydrogen phosphoric, dihydrogen phosphoric, phthalic, polygalacturonic, propionic, salicylic, seuric, succinie, sulfamic, sulfanilic, sulfonic, sulfuric, tannic, tartaric, teoclic, tolueene sulfonic, and the like. Pharmaceutically acceptable salts may be derived from amino acids, including but not limited to cysteine. Other pharmaceutically acceptable salts may be found, for example, in Stahl et al., Handbook of Pharmaceutical Salts: Properties, Selection, and Use, Wiley-VCH; Verlag Helvetica Chimica Acta, Zürich, 2002. (ISBN 3-906390-26-8). Pharmaceutically-acceptable cations include among others, alkali metal cations (e.g., Li+, Na+, K+), alkaline earth metal cations (e.g., Mg2+, Ca2+), non-toxic heavy metal cations and ammonium (NH4+) and substituted ammonium (R'NH4+), where R' is hydrogen, alkyl, or substituted alkyl, i.e., including, methyl, ethyl, or hydroxyethyl, specifically, trimethyl ammonium, triethyl ammonium, and triethanol ammonium cations). Pharmaceutically-acceptable anions include among other halides (e.g., Cl-, Br-), sulfate, acetates (e.g., acetate, trifluoroacetate), ascorbates, aspartates, benzoates, citrates, and lactate.

The compounds of this invention can contain one or more chiral centers. Accordingly, this invention is intended to include racemic mixtures, diastereomers, enantiomers, tautomers and mixtures enriched in one or more stereoisomer. The scope of the invention as described and claimed encompasses the racemic forms of the compounds as well as the individual enantiomers and non-racemic mixtures thereof.

DETAILED DESCRIPTION OF THE INVENTION

In general, the terms and phrases used herein have their art-recognized meaning, which can be found by reference to standard texts, journal references and contexts known to those skilled in the art. The following definitions are provided to clarify their specific use in the context of the invention.

"Supramolecular structure" refers to structures comprising an assembly of molecules. Supramolecular structures include assemblies of molecules, such as linear block copolymers having hydrophilic, hydrophobic and fluorophilic blocks, which are selectively oriented such that hydrophilic portions of the molecules are oriented outward toward a continuous aqueous phase, hydrophobic portions form an inner shell and fluorophilic portions of the molecules are oriented inward to form a fluoruous core. Supramolecular structures include assemblies of molecules such as linear block copolymers having hydrophilic, hydrophobic and fluorophilic blocks, which are selectively oriented such that hydrophilic portions of the molecules are oriented outward toward a continuous aqueous phase, and branched fluorophilic and hydrophobic portions are oriented inward to form a fluoruous core and hydrophobic intermediate shell. Supramolecular structures include, but are not limited to, micelles, vesicles, tubular micelles, cylindrical micelles, bilayers, folded sheets structures, globular aggregates, swollen micelles, and encapsulated droplets. Supramolecular structures of the present invention include self-assembled structures. Supramolecular structures may comprise the dispersed phase of a colloid, such as an emulsion or nanoeulsion.

"Semi-fluorinated" refers to chemical compounds having at least one fluorine atom, for example molecules having at least one carbon-fluorine bond.

Fluorocarbons as used herein refer to chemical compounds that contain at least one carbon-fluorine bond.

"Perfluorinated" and "perfluorocarbon" refers to chemical compounds that are analogs of hydrocarbons wherein all hydrogen atoms in the hydrocarbon are replaced with fluorine atoms. Perfluorinated molecules can also contain a number of other atoms, including bromine, chlorine, and oxygen. A bromine substituted perfluorocarbon is a perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a bromine atom. A chlorine substituted perfluorocarbon is a perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom. A chloro substituted perfluorocarbon is a perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom. Chlorine and bromine substituted perfluorocarbons perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom. A chloro substituted perfluorocarbon is a perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom. Chlorine and bromine substituted perfluorocarbons perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom. Chlorine and bromine substituted perfluorocarbons perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom. Chlorine and bromine substituted perfluorocarbons perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom. Chlorine and bromine substituted perfluorocarbons perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom. Chlorine and bromine substituted perfluorocarbons perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom. Chlorine and bromine substituted perfluorocarbons perfluorocarbon wherein one or more of the fluorine atoms have been replaced with a chlorine atom.

"Perhalogenated fluorous compound" refers to fluorophilic chemical compounds that are analogs of a substituted or unsubstituted hydrocarbon wherein the hydrogen atoms are replaced with halogen atoms, such as fluorine, chlorine and bromine. Perhalogenated fluorous compounds can also contain a number of other atoms, including oxygen, sulfur and nitrogen. Perhalogenated fluorous compounds include perfluorocarbons and substituted perfluorocarbons, such as chlorine substituted perfluorocarbons, bromine substituted perfluorocarbons and chlorine and bromine substituted perfluorocarbons.

"Emulsion" refers to a mixture of two or more immiscible substances, such as a mixture of two immiscible liquids. Emulsions are a type of colloid that comprise at least one dispersed phase dispersed in a continuous phase. Emulsions are broadly defined as two immiscible phases in which a first phase is dispersed within a second phase, such as a two-phase system in which one liquid is dispersed throughout a second liquid in the form of small droplets. The energy can be either supplied by mechanical equipment or the chemical potential inherent within the components. The two phases of an emulsion are generally referred to as the continuous phase and the dispersed phase, with the dispersed phase typically present as a smaller volume percentage. A dispersion of oil in water is referred to as an oil-in-water (o/w) emulsion. For o/w emulsions the emulsifying agent is typically more soluble in the aqueous phase. The reverse emulsion, water-in-oil, is abbreviated w/o and is stabilized by surfactants that are more stable in the oil phase. In an aqueous emulsion, the continuous phase is an aqueous solution.
Emulsions are not thermodynamically stable, but the stability can be improved by additives such as surfactants. As non-equilibrium systems, the formation of nanoemulsions generally requires an input of energy. High-energy emulsification methods commonly involve the introduction of mechanical shear through such equipment as high-shear stirers, high-pressure homogenizers, microfluidizers or ultrasound generators. A microfluidizer is the piece of equipment used in the pharmaceutical industry for the production of emulsions that works by dividing a stream of liquid into two parts, passing each through a narrow opening and then colliding the streams under high pressure. The high shear forces created by the collision provide very fine emulsions with generally narrow particle size distributions. In typical usage, a coarse emulsion (diameter > 1 µm) is first formed by some other method, and the size of that larger emulsion is reduced in the microfluidizer. The final droplet size and distribution shape will be dependent upon both the emulsion components (surfactant amount, oil volume percent, etc.) and the processing parameters (time, temperature, pressure etc.). As the desired droplet size decreases, the energy required for formation increases. Ultrasonic emulsification is also effective to reduce the size of emulsion droplets into the nanoscale. Emulsions can also be formed by changing the temperature of a mixture of immiscible liquids, for example by rapid cooling or heating to produce kinetically stable emulsions with small droplet sizes and narrow size distributions.

Emulsions include nanoemulsions comprising nanoscale droplets of one immiscible liquid dispersed within another. As used herein a nanoemulsion is a heterogeneous system composed of one immiscible liquid dispersed as droplets within another liquid, where the average droplet diameter is below 1000 nm.

"Flocculation" refers to a process in which clusters of two or more droplets behave kinetically as a unit, but individual droplets still maintain their identity. Flocculation may be reversible, or lead to coalescence, which is irreversible.

"Coalescence" is the collision, and subsequent irreversible fusion, of two droplets. The ultimate end of coalescence is complete phase separation. Flocculation precedes coalescence, so the same methods that are appropriate for prevention of flocculation also prevent coalescence. A thick, surfactant film adsorbed at the interface is often sufficient to prevent coalescence, whether in nano- or macro-emulsions.

"Ostwald ripening" refers to the growth in the size of emulsion droplets as the contents of one drop diffuse into another. The driving force for this growth is the difference in chemical potential between droplets, which is generally not substantial for droplets larger than 1 µm. Therefore, Ostwald ripening primarily affects nanoemulsions, and is an important factor for nanoemulsions for therapeutic applications.

"Polymer" refers to a molecule comprising a plurality of repeating chemical groups, typically referred to as monomers. A “copolymer”, also commonly referred to as a heteropolymer, is a polymer formed when two or more different types of monomers are linked in the same polymer. "Block copolymers" are a type of copolymer comprising blocks or spatially segregated domains, wherein different domains comprise different polymerized monomers. In a block copolymer, adjacent blocks are constitutionally different, i.e. adjacent blocks comprise constitutional units derived from different species of monomer or from the same species of monomer but with a different composition or sequence distribution of constitutional units. Different blocks (or domains) of a block copolymer may reside on different ends of a polymer (e.g. [A][B]), or may be provided in a selected sequence ([A][B][A][B]). "Diblock copolymer" refers to block copolymers having two different chemical blocks. "Triblock copolymer" refers to block copolymers having three different chemical blocks. Polymers of the present invention include block copolymers having a first block comprising a smaller polymer (e.g., 2 to 30 monomers), such as a fluorocarbon, including but not limited to, a fluorocarbon such as a fluorinated or perfluorinated alkane, a second interior hydrophobic block, and a third block comprising a larger polymer (e.g., 10-300) such as a PEG polymer having 10 to 270 monomers. Block copolymers of the present invention are capable of undergoing self-assembly to make supramolecular structures, such as encapsulated droplets. As used herein, the term block copolymer includes compositions comprising a first block comprising a PEG polymer conjugated to a second block comprising a hydrophobic polymer and further conjugated to a third block comprising a perfluorinated or fluorinated molecular domain, such as a perfluorinated or semifluorinated alkane or a perfluorinated or semi fluorinated tail. As used herein, the term block copolymer also includes functionalized block copolymers, such as copolymers having additional moieties for targeting a supramolecular structure to an active site, for stabilizing a supramolecular structure or for selecting the release kinetics of a supramolecular structure containing a fluorinated therapeutic compound.

As used herein “hydrophilic” refers to molecules and/or components (e.g., functional groups, blocks of block polymers, etc.) of molecules having at least one hydrophilic group, and hydrophobic refers to molecules and/or components (e.g., functional groups of polymers, and blocks of block copolymers etc.) of molecules having at least one hydrophobic group. Hydrophilic molecules or components thereof tend to have ionic and/or polar groups, and hydrophobic molecules or components thereof tend to have non-ionic and/or nonpolar groups. Hydrophilic molecules or components thereof tend to participate in stabilizing interactions with an aqueous solution, including hydrogen bonding and dipole-dipole interactions. Hydrophobic molecules or components tend not to participate in stabilizing interactions with an aqueous solution and, thus often cluster together in an aqueous solution to achieve a more stable thermodynamic state. In the context of block copolymers of the present invention, a hydrophilic block is more hydrophilic than a hydrophobic group of an amphiphilic block copolymer, and a hydrophobic group is more hydrophobic than a hydrophilic block of an amphiphilic polymer.

As used herein “fluorophilic” refers to molecules and/or components (e.g., functional groups, blocks of block polymers etc.) of molecules having at least one fluorophilic group, and fluorophobic refers to molecules and/or components (e.g., fluorinated or perfluorinated alkane, etc.) of molecules having at least one fluorophobic group. Fluorophilic molecules or components thereof tend to participate in stabilizing interactions with a fluorous phase. Fluorophilic groups useful in block copolymers compounds of the invention include, but are not limited to, fluorocarbon groups, perfluorinated groups and semifluorinated groups.

In the context of the present invention the term patient is intended to include a subject such as an animal. Patient includes a mammal, for example human subject. Patient includes a subject undergoing a medical procedure, such as undergoing the administration of anesthesia or other medical procedure.

Before the present methods are described, it is understood that this invention is not limited to the particular methodology, protocols, cell lines, and reagents described, as these may vary. It is also to be understood that the terminology used herein is for the purpose of describing particular
embodiments only, and is not intended to limit the scope of the present invention which will be limited only by the appended claims.

It must be noted that as used herein and in the appended claims, the singular forms “a”, “an”, and “the” include plural reference unless the context clearly dictates otherwise. Thus, for example, reference to “a cell” includes a plurality of such cells and equivalents thereof known to those skilled in the art, and so forth. As well, the terms “a” (or “an”), “one or more” and “at least one” can be used interchangeably herein. It is also to be noted that the terms “comprising”, “including”, and “having” can be used interchangeably.

Unless defined otherwise, all technical and scientific terms used herein have the same meanings as commonly understood by one of ordinary skill in the art to which this invention belongs. Although any methods and materials similar or equivalent to those described herein can be used in the practice or testing of the present invention, the preferred methods and materials are now described. All publications mentioned herein are incorporated herein by reference unless the context clearly dictates otherwise. Thus, for example, reference to “a cell” includes a plurality of such cells and equivalents thereof known to those skilled in the art, and so forth. As well, the terms “a” (or “an”), “one or more” and “at least one” can be used interchangeably herein. It is also to be noted that the terms “comprising”, “including”, and “having” can be used interchangeably.

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The invention may be further understood by the following non-limiting examples.

Example 1: Emulsion-Based Formulations of Propofol

This example provides a description of compositions and physical properties of specific examples of emulsions useful in the present formulations and therapeutic methods. In addition, the results of animal tests are described demonstrating clinical efficacy for examples of the present formulations and therapeutic methods. The description and experimental results are divided into two analysis sections (Analysis Section No. 1 and Analysis Section No. 2) which taken together demonstrate useful properties and applications of certain embodiments of the present invention.

Analysis Section No. 1

Commercial propofol (Diprivan) consists of an Intralipid® emulsion of the active principle 2,6-diisopropylphenol. This emulsion is used extensively in anesthesiology practice to induce and maintain general anesthesia. Propofol is also used for procedural sedation (e.g. colonoscopy) and for sedation in intensive care units.

The current formulation of propofol is subject to a variety of problems, one of the most important being the ability to support bacterial and fungal growth. This is due to the main ingredient of Intralipid®: soybean oil or a similar lipid. Because of the risk of contamination, tubing and open vials of propofol must be replaced every twelve hours. In addition, infusion at a high rate or as a large bolus can lead to lipid intolerance, and may contribute to ‘propofol infusion syndrome’, a rare but serious complication that limits its use in the intensive care unit. The development of a non-lipidic propofol emulsion would address these problems and thus would be an important advance.

The present example demonstrates the ability of semifluorinated surfactants to stabilize emulsions of various
the present emulsions are compatible with formulation using 1 to 20% PFOB. As shown in FIG. 2, Formulation containing a linear triblock copolymer is useful for formulation containing a linear triblock copolymer is useful for enhancing the emulsion stability. Different polymer architectures have been tested and all of them are remarkably effective, although with some differences. For instance, addition of a perhalogenated fluorous compound to a formulation containing a linear triblock copolymer is useful for generating stable emulsions with propofol.

The emulsions described in this example are much simpler in composition than the current commercial propofol and offer the advantage that they do not support microbial growth. In the new emulsions, simple saline can be used to ensure isotonicity instead of glycerol, a chemical required for Intralipid® stability. Importantly, the new emulsions are as effective as the currently used propofol. Emulsion with Linear Semifluorinated Triblock Copolymer and Perhalogenated Fluorous Compound

The physical properties of propofol emulsions comprising the linear semifluorinated triblock copolymer (M1H10F8) and perfluorooctylbromide (PFOB) were characterized.

Specifically, the following formulations were evaluated.

Formulation 1: 15.97 mL saline, 280 mg M1H10F8, 0.18 mL propofol, 0.850 mL PFOB
Formulation 2: 15.12 mL saline, 280 mg M1H10F8, 0.18 mL propofol, 1.7 mL PFOB
Formulation 3: 13.42 mL saline, 280 mg M1H10F8, 0.18 mL propofol, 3.4 mL PFOB

FIG. 2 provides a plot showing the mean droplet diameter (nm) for the emulsions corresponding to Formulations 1, 2 and 3 evaluated as a function of time (days). In FIG. 2, Formulation 1 corresponds to 5% PFOB, Formulation 2 corresponds to 10% PFOB and Formulation 3 corresponds to 20% PFOB. As shown in FIG. 2, formulations 1-3 formed stable emulsions with mean droplet diameters of between about 210 and 250 nm. Over a period of about 28 days, the mean droplet diameter of Formulation 1 increased to about 375 nm, while the mean droplet diameters of Formulations 2 and 3 increased to about 300 nm. The results demonstrate the present emulsions are compatible with formulation using saline solution, which has particular relevance for clinic use.

Animal Studies

FIGS. 3 and 4 show the results of animal studies for the administration of propofol emulsions. All animal studies were approved by the University of Wisconsin Animal Care and Use Committee, Madison, Wis., and were performed in accordance with the guidelines laid out in the Guide for the Care and Use of Laboratory Animals published by the National Research Council.

Experiments to measure loss and recovery of the righting reflex were carried out in six male Sprague-Dawley rats (Harlan Spraque-Dawley, Inc., Indianapolis, Ind.) weighing approximately 280 g. The rats were received from the supplier with a surgically implanted jugular catheter. Different propofol formulations were tested: 1) lipid-based propofol formulation as in current clinical use (Propofol: Diamonds); 2) Formulation 5 (B8: Squares; 16.82 mL saline, 420.5 mg (25 mg/ml) M1H10F8, 0.18 mL propofol); 3) Formulation 4 (L3: Triangles; 16.82 mL saline, 240.5 mg M1H10-O-F3 (25 mg/ml)), 201.8 g E80 (12 mg/mL), 0.18 mL propofol) and 4) Formulation 3 (F8: Xs; 13.42 mL saline, 280 mg M1H10F8, 0.18 mL propofol, 3.4 mL PFOB). For each formulation, five different doses were administered three times each.

The propofol emulsions were administered by first restraining the rat with a towel. The plug placed at the end of the catheter was then removed and replaced with a 23-gauge needle connected to an insulin-type syringe. To remove the heparin-based fill solution and check that no blockage was obstructing the catheter, the syringe plunger was slowly withdrawn until blood filled the catheter. The 23-gauge needle was then connected to the syringe containing the propofol emulsion to be tested. The rat was then placed in a transparent cage for observation. Forty µl of the emulsion, corresponding to the volume of the catheter, was injected to prime the catheter and then the administration of the emulsion was started. The emulsion injection rate was controlled through an infusion pump (11 plus; Harvard Apparatus, Holliston, Mass.). A bolus dose was delivered within 20 s regardless of the volume. Loss of righting reflex (LORR) was evaluated by rolling the rat onto its back and observing whether the animal was able to right itself. The times to achieve and to recover from LORR were recorded.

When the rat completely recovered from LORR, the catheter was flushed with 0.04 ml of a normal saline solution to remove the residual emulsion and then refilled with 0.04 ml of a heparin-based fill solution. The end of the catheter was sealed with a sterile plug.

FIG. 3 provides plots of time to LORR (s) as a function of dose (mg/kg). FIG. 4 provides plots of time to Time to Return of Righting Reflex (s) as a function of dose (mg/kg). Data are plotted as time to loss or recovery of righting reflex as a function of drug dose, expressed on a mg/kg basis for the propofol component of the nanoemulsion. The x-axis intersection is the calculated ED50 for inducing LORR as a surrogate for unconsciousness. All three formulations proved effective with similar ED50 values. The data shown in FIGS. 3 and 4 indicate efficacies of the present emulsions having semifluorinated block copolymer are comparable to the lipid-based propofol formulation currently in use.

Experimental Section

Structures of linear, branched, and miktoarn amphiphiles with associated nomenclature are shown below.

Linear Amphiphiles

M1H10-O-F3 (L3)

[Diagram of Linear Amphiphile]

M1H10F8 (F8)

Miktoarn amphiphile

M1H10F8 (B8)

[Diagram of Miktoarn Amphiphile]
Mx refers to the mPEG hydrophilic block with x being the average molecular weight in thousands. For non-linear amphiphiles, µ specifies miktoarm architecture, respectively. H # corresponds to the number of hydrogenated carbon atoms and F # corresponds to the number of fluorinated carbon atoms. For the linear polymers, the presence or absence of —O— indicates the presence or absence of an ether linkage between the blocks.

Materials

All fluorinated compounds were obtained from SynQuest Laboratories, Inc. (Alachua, Fla., USA), Lipoid ESQ was purchased from Lipoid GmbH (Ludwigshafen, Germany). All solvents were of ACS grade or higher and were purchased from Sigma-Aldrich (St. Louis, Mo., USA). All other reagents were purchased from Sigma Aldrich (St. Louis, Mo., USA) and were used as received, unless otherwise specified.

Chromatographic separations were performed using Silicycle 60 Å SiO₂. Surfactants were purified automated flash chromatography using a CombiFlash® Rf 4x system (Teledyne Iseco, Lincoln, Nebr., USA) equipped with a Gold C-18 aqueous reverse phase cartridge. ¹H- and ¹³F-NMR spectra were obtained on Varian Unity-Inova 400 and Unity-Inova 500 spectrometers using deuteriochloroform (CDCl₃) as the solvent with TMS as an internal reference.

Scheme 1. Synthesis of linear and dibranched alcohols

Radical Synthesis

\[
\begin{align*}
\text{HO} & \quad \text{F(CF₂)₃} \\
\text{80° C., overnight} & \\
\text{Zn powder} & \quad \text{AsOH} \\
\text{16 h, rt} & \\
\text{HO} & \quad \text{CF₂OH} \\
\text{2, HO-H₁₀F₈} & \\
50\% \text{ yield over 2 steps} & \\
\end{align*}
\]

Anionic Synthesis

1. MsCl, TEA, DCM
2. F₃H₁₀-OH, NaH, THF
3. BH₃, THF
4. NaOH, H₂O₂

Scheme 2. Synthesis of miktoarm alcohols

Linear alcohols. HO-H₁₀F₈ (2): To a dry 10 mL round-bottom flask were added 1.02 mL (5.75 mmol) 9-decen-1-ol and 1.34 mL (5.0 mmol) perfluorooctyl iodide. The mixture was degassed for 30 minutes before 8.2 mg (0.05 mmol) AIBN were added and the mixture slowly heated to 80°C. The reaction was allowed to run overnight. The reaction was then cooled to room temperature, diluted with 100 mL DCM and washed with 3x50 mL aliquots saturated ammonium chloride solution, dried over magnesium sulfate and then reduced to a minimum volume under reduced pressure. The mPEG-OMs was then precipitated with cold ether, vacuum filtered, and freeze dried from 50/50 DCM/benzene to give a white, crystalline product in 67% yield mPEG₁₂₀₀-OMs.

Method

mPEG mesylate (Mx-OMs). To a dry 100 mL round-bottom flask charged with argon were added 50 mL DCM and 5 g monomethyl poly(ethylene glycol) alcohol 5 g M₃-OH. The mixture was cooled to 0°C, before adding 2 mL TEA, which was allowed to stir for 30 minutes before 1 mL methanesulfonyl chloride was added. The reaction was allowed to stir overnight as it warmed to room temperature. The reaction was then diluted with 100 mL DCM and washed with 3x50 mL aliquots saturated ammonium chloride solution, dried over magnesium sulfate and then reduced to a minimum volume under reduced pressure. The mPEG-OMs was then precipitated with cold ether, vacuum filtered, and freeze dried from 50/50 DCM/benzene to give a white, crystalline product in 67% yield mPEG₁₂₀₀-OMs.

mPEG₁₂₀₀-OMs MALDI: Distribution centered on [M+Na⁺]=1063, PDI of starting mPEG 1.27. NMR: ¹H NMR (400 MHz, CDCl₃): δ 4.38 (m, 2H), 3.82 (m, 1H), 3.77 (m, 2H), 3.64 (m, 89H), 3.55 (m, 2H), 3.47 (m, 1H), 3.38 (s, 3H), 3.09 (s, 3H).

Linear alcohols. HO-H₁₀F₈ (2): To a dry 10 mL round-bottom flask were added 1.02 mL (5.75 mmol) 9-decen-1-ol and 1.34 mL (5.0 mmol) perfluorooctyl iodide. The mixture was degassed at room temperature with argon for 45 minutes before 8.2 mg (0.05 mmol) AIBN were added and the mixture slowly heated to 80°C while being very rapidly stirred with a small stir bar. This reaction was allowed to run overnight. The reaction was then cooled to room temperature, diluted with 100 mL DCM, washed with 1x50 mL aliquot each Na₂S₂O₃ and brine. The organic layers were dried over MgSO₄ and condensed under reduced pressure to give an off-white solid (1). This was then dissolved in 10 mL acetic acid and stirred with 0.98 g zinc powder for 24 hours...
open to the air. The reaction was then quenched with 200 mL saturated NaHCO₃ solution and extracted with 300 mL DCM. The organic layers were then washed with 1×100 mL aliquot each saturated NaHCO₃ solution and brine and then dried over MgSO₄ and concentrated under reduced pressure to give a white solid. The solid was recrystallized twice from hot toluene to give pure (2) HO-H₁₀-O-F₃ in 48% yield. NMR: ¹H NMR (400 MHz, CDCl₃): δ 5.81 (ddt, J=6.5, 10, 6.5 Hz, 1H), 4.99 (ddt, J=16.5, 2, 1 Hz, 1H), 4.93 (ddt, J=10, 2, 1 Hz, 1H), 4.22 (t, J=7 Hz, 2H), 3.00 (s, 3H), 2.04 (qt, J=6.5, 1 Hz, 2H), 1.60 (q, J=7 Hz, 2H), 1.41-1.29 (m, 1OH). ¹⁹F NMR (376 MHz, CDCl₃): δ -81.15 (3F), -114.77 (10F). HO-H₁₀-O-F₃ NMR: 1H NMR (400 MHz, CDCl₃): δ 7.48 (m, 2H), 7.36 (m, 3H), 5.50 (s, 1H), 4.12 (dd, J=12.0, 1.4 Hz, 2H), 4.02 (dd, J=12.0, 1.3 Hz, 2H), 3.54 (dt, J=10.6, 1.5 Hz, 1H), 3.36 (d, J=10.5 Hz, 1H). 5-(decyloxy)-2-phenyl-1,3-dioxan-5-ol (4) was dissolved in 80 mL anhydrous toluene and 2.30 g crushed NaH was added. Reaction fitted with Dean-Stark trap and heated to reflux for 6 hours. The reaction was then cooled, and 7.41 decyl methane sulfonate was added as a solution in toluene (20 mL). The reaction was then heated to reflux for 5 days. The reaction was then cooled to room temperature, diluted with 100 mL water, and concentrated under reduced pressure. Crude oil purified by flash column (5% ethyl acetate in hexanes) to obtain 3.309 g 5-(decyloxy)-2-phenyl-1,3-dioxan-5-ol (4) in 80% yield. The product was then purified by column chromatography (4% ethyl acetate in hexanes) to obtain 3.21 g of 5-(decyloxy)-2-phenyl-1,3-dioxan-5-ol (4). 1H NMR (400 MHz, CDCl₃): δ 7.50 (m, 2H), 7.33 (m, 3H), 5.54 (s, 1H), 4.31 (dd, J=12.4, 1.2 Hz, 2H), 4.02 (dd, J=12.4, 1.6 Hz, 2H), 3.53 (dt, J=6.8 Hz, 2H), 3.24 (t, J=2.0 Hz, 1H), 1.65 (p, J=6.8 Hz, 2H), 1.28 (m, 14H), 0.88 (t, J=6.8 Hz, 3H).
bath to warm to room temperature. The reaction was then diluted with DCM (50 mL) and washed with 3 aliquots saturated NH₄Cl solution, dried over MgSO₄, and solvents removed under reduced pressure to give a pale yellow oil. 7 7.102 g (95% yield). 7 ¹H NMR (400 MHz, CDCl₃): δ 7.33 (m, 5H), 4.54 (dd, J=12.1, 2.3 Hz, 2H), 4.39 (dd, J=10.9, 3.8 Hz, 1H), 4.27 (dd, J=10.8, 5.7 Hz, 1H), 3.70 (p, J=4.7 Hz, 1H), 3.55 (m, 4H), 3.00 (s, 3H), 1.56 (p, J=6.8 Hz, 2H), 1.28 (m, 14H), 0.88 (t, J=6.8 Hz, 3H).

(2-(deoxyloxy)-(1H,1Hperfluoronylonyloxy)propoxy) methyI (8): 3.160 g was dissolved in anhydrous BTF and 5.12 g F8H11OH added, and flask flushed with 667 mg NaH were slowly added, and reaction heated to reflux for 3 days. Reaction was quenched dropwise with H₂O and further diluted with water and DCM and layers separated. Organics dried over MgSO₄ and solvents evaporated under vacuum. Purified by column chromatography (5% ethyl acetate in hexanes) to obtain pure 8 in 67% yield (3.985 g). ³¹P NMR (400 MHz, CDCl₃): δ 140.6 (J=9.4 Hz, 2H), 3.67-3.62 (m, 80H), 3.59-3.51 (m, 7H), 3.46 (m, 1H), 3.38 (s, 3H), 1.57 (p, J=7.2 Hz, 2H), 1.26 (m, 1H), 0.88 (t, J=6.8 Hz, 3H).

7.102 g (95% yield). 7 ¹H NMR (400 MHz, CDCl₃): δ 7.33 (m, 5H), 4.54 (dd, J=12.1, 2.3 Hz, 2H), 4.39 (dd, J=10.9, 3.8 Hz, 1H), 4.27 (dd, J=10.8, 5.7 Hz, 1H), 3.70 (p, J=4.7 Hz, 1H), 3.55 (m, 4H), 3.00 (s, 3H), 1.56 (p, J=6.8 Hz, 2H), 1.28 (m, 14H), 0.88 (t, J=6.8 Hz, 3H).

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Emulsion Preparation
Surfactant with or without E80 additive emulsion. To a 50 mL falcon tube were added 16.82 mL normal saline, 25 mg mL⁻¹ surfactant and, if included, 12 mg mL⁻¹ Lipoid E80. This was vortexed for 1 minute and sonicated for 30 minutes with heating. The resulting solution was allowed to cool to room temperature and then 0.18 mL propofol was added and the mixture homogenized by high-speed mixing (21,000 rpm) for 1 minute. The crude emulsion was then refined by microfluidization (5,000 psi) for 1 minute. The resulting emulsion was then filtered with a 0.45 µm nylon filter and stored at 4° C.

Analysis Section No. 2
Propofol is the most common agent for induction of general anesthesia in the United States. In addition, it is commonly used for maintenance of anesthesia as well as sedation in the operating room and intensive care unit. The formulation available clinically (Diprivan®) is a lipid emulsion of 1% propofol with 10% soybean oil, 1.2% egg yolk lecithin, and 2.25% glycercol. This formulation is clinically effective but it does have several drawbacks, including the allowance of microbial growth, effects related to hyperlipidemia (elevated triglycerides and propofol infusion syndrome), and pain on injection. Although minor, anaphylaxis has also been of concern. Because of these issues, many attempts have been made to reformulate the drug. These attempts have included the addition of preservatives and anti-microbials, variations of oil and lecithin content, changes in size of triglycerides, and a host of new solvents.

This in set of experiments, we studied four propofol nanoe­mulsions using novel surfactants, and compared their anesthetic effects to those of Diprivan® in rats. In addition, we tested whether a bolus of Intralipid® administered during the recovery phase would accelerate emergence from anesthesia.
All animal studies were approved by the University of Wisconsin Animal Care and Use Committee, Madison, Wis. Experiments to measure loss and recovery of the righting reflex were carried out in six male Sprague-Dawley rats weighing approximately 280 g. The rats were received from the supplier with a surgically-implanted jugular catheter. Five different propofol formulations were tested: 1) Diprivan®; 2) lipid-free formulation using a semihomogenized surfactant and egg lecithin designated L3; 3) lipid-free formulation using a semihomogenized surfactant designated BS; 4) lipid-free formulation using a semihomogenized surfactant and PFOB designated F8; 5) lipid-free formulation using only Lipoid E80 designated L80. For each formulation, five different bolus doses ranging from 5-15 mg/kg were administered 5 times each over 20 s using a syringe pump. In all cases, the rats received only one dose of anesthetic per day. Subsequently, the anesthetic effects of BS and Diprivan® were tested for reversibility using an Intralipid® bolus after an induction dose. Intralipid® doses from 3.75-15 ml/kg were tested in combination with 15 mg/kg of BS or Diprivan®.

Four of the five formulations showed efficacy in causing loss of the righting reflex. The one exception was L80, which did not induce anesthesia at doses up to 15 mg/kg. The other formulations all induced LORR, all animals regained righting reflex, and no ill effects were observed during or after the anesthetic period. To compare potency of induction doses between the formulations, time to recovery of righting reflex was plotted vs log dose. For each data set, the linear regression line crossing the x-axis was considered the threshold dose for causing loss of righting reflex. There were no significant differences between the threshold doses for the four drugs: 5.2, 6.0, 5.5, and 6.8 mg/kg for Diprivan®, L3, BS, and F8 respectively. Using a similar method for evaluating the effect of Intralipid® bolus, time to recovery of righting reflex was plotted vs log dose with the slope of the linear regression line representing clearance. A 39% (p<0.014) and 51% (p<0.046) reduction in slope were seen for Diprivan® and BS, respectively.

The three lipid-free fluoro-polymer-based formulations of propofol all showed similar efficacy, potency, and duration in producing and maintaining anesthesia with bolus dosing, comparable to Diprivan. Additionally, clearance of propofol from its effect site was accelerated with Intralipid® after an induction dose. These lipid-free formulations have the potential to avoid complications related to microbial growth and hyperlipidemia that are seen with the currently available formulation of propofol. Further study is indicated to determine toxicity and side effect profiles of these novel surfactant formulations before they can be considered for clinical use.

Introduction
Propofol is commonly used for induction and maintenance of general anesthesia, and for sedation in the operating room and intensive care unit. Initially tested for administration in Cremophor EL, the formulation now available clinically for evaluating the effect of Intralipid® bolus, time to 35 mg/kg of BS or Diprivan®.

The use of propofol in intravenous anesthetic agents is based upon the observation that propofol is a potent and short-acting sedative which acts on the central nervous system to produce a state of general anesthesia. Propofol has been used for a variety of clinical applications, including induction of anesthesia, maintenance of anesthesia, and recovery of righting reflex was plotted vs log dose with the slope of the linear regression line representing clearance. A 39% (p<0.014) and 51% (p<0.046) reduction in slope were seen for Diprivan® and BS, respectively.

The three lipid-free fluoro-polymer-based formulations of propofol all showed similar efficacy, potency, and duration in producing and maintaining anesthesia with bolus dosing, comparable to Diprivan. Additionally, clearance of propofol from its effect site was accelerated with Intralipid® after an induction dose. These lipid-free formulations have the potential to avoid complications related to microbial growth and hyperlipidemia that are seen with the currently available formulation of propofol. Further study is indicated to determine toxicity and side effect profiles of these novel surfactant formulations before they can be considered for clinical use.

Methods
Experiments were carried out in two phases. The purpose of the first phase was to demonstrate the efficacy of L3, BS, and F8 to produce anesthesia; to determine a threshold dose for causing loss of righting reflex (LORR) in the rat; and to test for adverse effects of the drugs—all in comparison to Diprivan®. The purpose of the second phase was to determine the effect of a bolus of Intralipid® on the anesthetic effects of BS and Diprivan®.

Many different formulations of propofol have been studied in an attempt to remedy these issues. Preservatives and anti-microbial agents such as EDTA and sodium metabisulfite have been added. (Baker, Thompson) The oil and lecithin contents have been varied. (Song) Different sizes of triglycerides and new solvents have been tested. (Ran, Egan) Propofol’s interaction with local endothelium, caused either by free propofol in the aqueous phase or by the drug being released rapidly from the oil phase, has been implicated in causing pain with injection. (Damitzl, Dobey, Ohmizo) Therefore, alternative emulsions have been developed to minimize the free concentration in an attempt to minimize this problem. (Cai, Damitz2) Produgs of propofol such as fospropofol are clinically available and have decreased pain on injection but have slower onset and prolonged elimination half-life. (Pergolizzi) Recently, Aquafol (Daewon Pharmaceutical Co., Ltd., Seoul, Korea), a 1% propofol micronemulsion with 10% purified poloxamer 188 (PP188) and 0.7% poly-ethylene glycol 660 hydroxystearate (using no lipid), has become clinically available in some parts of the world. (Jung, Sim, Lee)

In this set of experiments, we studied in rats three propofol nonemulsions prepared using novel semihomogenized surfactants, and compared their anesthetic effects to formulations containing only the classical surfactant Lipoid E80 and the clinically used formulation of Diprivan®. Semihomogenized-surfactant based emulsions have been studied as blood substitutes and also used for intravenous drug delivery, including intravenous delivery of the inhalational anesthetic sevoflurane. (Riess1, Riess2, Kraftl, Fast) Semihomogenization surfactants were chosen for their unique architecture (lipophilic and fluorophilic blocks) and designed to eliminate the need to add soybean oil to the emulsion. The lipophilic moiety was intended to stabilize the dissolved propofol, and the fluorophilic moiety to stabilize the nanoemulsion.

In addition to testing these emulsions for stability and efficacy, we tested whether a post-induction bolus of Intralipid® would accelerate recovery from the anesthetic effects of propofol, a highly lipid-soluble drug, as it does for the toxic effects of several lipid-soluble drugs including bupivacaine. (Weinberg/Vadel/Hancouer) The rationale for these studies is that the octanol:water partition coefficient (log P) of propofol is 3.79 (Babu), which makes it even more lipid soluble than bupivacaine (log P 3.41). (Hansch) If the lipid solubility of propofol causes a decreased effect site concentration with lipid infusion through partitioning, then the duration of anesthesia caused by propofol may be reduced with a lipid infusion.

Methods
Experiments were carried out in two phases. The purpose of the first phase was to demonstrate the efficacy of L3, BS, and F8 to produce anesthesia; to determine a threshold dose for causing loss of righting reflex (LORR) in the rat; and to test for adverse effects of the drugs—all in comparison to Diprivan®. The purpose of the second phase was to determine the effect of a bolus of Intralipid® on the anesthetic effects of BS and Diprivan®.

Surfactants
The semihomogenized surfactants M11H11O-F5 and M11pH10F8 were used in the L3 and BS emulsions, respectively, and the classical surfactant M5diH10, and the semihomogenized surfactant M11H10F8 were used in the F8 emulsion. These emulsions were synthesized as previously reported. (Tucker)
Sigma Aldrich Co. (Milwaukee, Wis.) was added to the polymer solutions for a total volume of 17 mL. The high-speed homogenizer (Power Gen 500) from Fisher Scientific (Hampton, N.H.) and the microfluidizer (model 110 S) from Microfluidics Corp. (Newton, Mass.) were first cleaned with 70% and 100% ethanol, followed by 70% and 100% methanol, and finally with three rinses of Millipore water. Once prepared, each emulsion mixture was then homogenized with the high-speed homogenizer for 1 min at 21,000 rpm at room temperature. The crude emulsion was then microfluidized for 1 min at 5,000 psi with the cooling bath kept at 10° C. The final emulsion was then filtered with a 30 mm dia., 0.45 µm nylon filter and stored in 45 mL plastic centrifuge tubes from Corning Inc. (Corning, N.Y.) at 4° C. After preparation and filtration of the emulsions, the emulsion droplet sizes were measured by dynamic light scattering (NICOMP 380ZLS) from Particle Sizing Systems (Santa Barbara, Calif.). An aliquot of the emulsion, approximately 150 µL, was diluted in 3 mL of Millipore water to achieve an intensity factor range of 300-350. Each measurement was run for 5 minutes at room temperature and repeated in triplicate. The data were analyzed by Gaussian analysis and reported as a volume-weighted average diameter. The emulsion errors for all polymers were taken as an average of the standard deviations of each individual measurement.

Emulsions

All emulsions were prepared by combining the surfactant, additives and propofol in water (with salt or glycerol for isotonicity). B8, L3, and M5diH10 surfactant solutions were prepared as 25 mg/mL solutions by direct dilution of lyophilized solid in sterile, normal saline solution to a total volume of 16.82 mL. The emulsion L30, containing only Lipoid E80, from Lipoid GmbH (Ludwigshafen, Germany), were prepared by dissolution of Lipoid E80 at a concentration of 12 mg/mL in 16.82 mL double-distilled water with added glycerol for isotonicity. L3 also contained 12 mg/mL Lipoid E802. The F8 surfactant solution was prepared as a 16 mg/mL solution in 13.42 mL normal saline with 3.4 mL perfluorooctyl bromide (PFOB) from Synquest Labs (Alachua, Fla.). The solutions were sonicated until completely dissolved. 0.18 mL volume of 2,6-diisopropylphenol from Animal Studies

All animal studies were approved by the University of Wisconsin Animal Care and Use Committee, Madison, Wis., and were performed in accordance with the guidelines laid out in the Guide for the Care and Use of Laboratory Animals published by the National Research Council. Phase I and 2 experiments were carried out in six male Sprague-Dawley rats (Harlan Spraque-Dawley, Inc., Indianapolis, Ind.) weighing approximately 280 g. The rats were received from the supplier with a surgically implanted jugular catheter. In all cases, the rats received only one dose of anesthetic per day. In phase I, experiments to measure loss and recovery of righting reflex were conducted using five different propofol formulations: 1) Diprivan®; 2) L3; 3) B8; 4) F8; and 5) L30. For each of the first three formulations, five different doses (5-15 mg/kg) were administered five times each. For F8 each of the five doses was administered three times each. For L30,
the highest dose (15 mg/kg) was tested five times. Since this dose did not lead to LORR, a limited number of lower doses were studied, and none led to LORR. Dosing was based on previously published data for propofol in rats. (Adam, Glen, Brammer).

The propofol emulsions were administered by first weighing the rat and then restraining it with a towel. The plug placed at the end of the catheter was then removed and replaced with a 23-gauge blunt tip needle connected to an insulin-type syringe. To remove the heparin-based fill solution and check that no blockage was obstructing the catheter, the syringe plunger was slowly withdrawn until blood filled the catheter. The 23-gauge blunt tip needle was then removed and the catheter was connected using a 23-gauge connector tip to the tubing and syringe containing the propofol emulsion to be tested. The rat was placed in a transparent cage for observation. Forty µl of the emulsion, corresponding to the volume of the catheter was injected to prime the catheter and then the administration of the emulsion was started. The emulsion injection rate was controlled through an infusion pump (11 plus; Harvard Apparatus, Holliston, Mass.). A bolus dose was delivered over 20 s regardless of the dose. LORR was evaluated by rolling the rat onto its back and observing whether the animal was able to right itself. The times to achieve and to recover from LORR were recorded. When the rat completely recovered from LORR, the catheter was flushed with 40 µl of 0.9% saline solution to remove the residual emulsion and then refilled with 40 µl of a heparin-based fill solution. The end of the catheter was sealed with a sterile plug.

In phase 2, experiments were performed to determine the effect of an Intralipid® bolus on the anesthetic effects of Diprivan® and BS were conducted. For both, three different doses (7.5-15 mg/kg) were administered five times each. The three doses chosen reliably caused LORR with both emulsions as determined in phase 1. In the same fashion as in phase 1, the rats were restrained and connected to the tubing and syringe containing the propofol emulsion. Procedures for bolus dose administration and determination of loss and recovery of righting reflex were carried out as in phase 1. Sixty seconds after starting the bolus propofol dose, the animals' catheters were connected to tubing and a syringe containing Intralipid® (20% lipid emulsion). A bolus of Intralipid® was then administered over 60 seconds. For the highest propofol dose administered, three different Intralipid® bolus doses were administered five times each (3.75-15 ml/kg). For the two decreased doses of propofol only the highest dose of Intralipid® was administered. Dosing was based on previously published data utilizing lipid for treatment of drug toxicity in rats. (Jamaty, Perez, Hiller, Di Gregorio, Weinberg/Vanderpuye).

Statistics

Comparisons were made using unpaired t-tests. Differences were considered significant at a level of p<0.05. Results

Emulsion Stability

In an effort to eliminate any added soybean oil from the developed propofol emulsions, semi-fluorinated surfactants were investigated for their ability to solubilize propofol (hydrophobic moiety) and stabilize the nanodroplet (fluorinated moiety). It was found that BS formulation-containing only M1P10H10F8 surfactant, as shown in FIG. 5, and propofol dispersed in normal saline-formed an emulsion stable for 42 days with a growth rate of 3.60 nm/day. A similar formulation using M1H10-O-F3 failed to produce a stable emulsion. As shown in FIG. 5, the stable formulation L3 utilized M1H10-O-F3 and Lipoid E80 as equimolar co-surfactants, was stable for 406 days, with a growth rate of 0.02 nm/day.

The results of further investigations into the emulsion formulation are shown in FIG. 6. It was found that the classical (hydrophobic-lipophilic) surfactant M59H10 did emulsify propofol and was stable for 21 days with a growth rate of 12.52 nm/day, but the emulsion rapidly grew in size. Lipoid E80—the surfactant used in Diprivan®—also formed stable emulsions, when glycerol instead of salt was used to achieve isotonicity. The emulsion was stable for 154 days with a growth rate of 0.50 nm/day. The final emulsion formulation investigated utilized a linear, semihalogenated surfactant M1H10F8, structurally similar to L3, but incorporated a fluorinated stabilizer (perfluorooctyl bromide, PFOB) instead of a phospholipid co-surfactant. This emulsion was found to be stable for 119 days with a growth rate of 1.65 nm/day.

Phase 1-Emulsion Efficacy

The L80 caused only mild sedation and failed to cause LORR up to a propofol dose of 15 mg/kg.

The five bolus doses tested of Diprivan®, L3, B8 and F8 were 5, 6.25, 7.5, 10 and 15 mg/kg. All three formulations proved effective in causing LORR, as shown in FIG. 7. F8 proved to be effective at inducing anesthesia, but only at higher doses (compared to BS, L3 and Diprivan) and with prolonged duration at the highest, 15 mg/kg, dose.

Data are plotted as time to loss or recovery of righting reflex as a function of drug dose, expressed on a mg/kg basis for the propofol component of the nanoemulsion. The x-axis intersection is the calculated threshold dose for inducing LORR as a surrogate for unconsciousness. (Liao)

There was no significant difference between threshold doses of Diprivan® and BS. The L3 threshold dose was slightly, but significantly higher. No ill effects were seen in the rats acutely, or after >10 doses over a two week period.

Table 1 shows that for the three doses that reliably caused LORR, time to recovery of righting reflex was significantly longer for Diprivan® compared to L3 and B8.

<table>
<thead>
<tr>
<th>TABLE I</th>
<th>Duration of Anesthesia versus Dose for Diprivan, L3, and B8</th>
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</thead>
<tbody>
<tr>
<td></td>
<td>Duration of anesthesia (s)</td>
</tr>
<tr>
<td></td>
<td>7.5 mg/kg</td>
</tr>
<tr>
<td>Diprivan®</td>
<td>157.60 ± 43.59</td>
</tr>
<tr>
<td>L3</td>
<td>65.33 ± 33.97</td>
</tr>
<tr>
<td>B8</td>
<td>189.67 ± 168.94</td>
</tr>
</tbody>
</table>

For 7.5 mg/kg doses, duration of anesthesia of L3 was significantly shorter (p=0.0050) than Diprivan®; B8 was not significantly different from L3 and Diprivan® or L3. For 10 mg/kg doses, duration of anesthesia of L3 and B8 were significantly shorter (p=0.0034 and p=0.0067, respectively) than Diprivan®; B8 and L3 were not significantly different from one another. For 15 mg/kg doses, duration of anesthesia of L3 and B8 were significantly shorter (p=0.0108 and p=0.0151, respectively) than Diprivan®; B8 and L3 were not significantly different from one another.

Phase 2-Intralipid® Studies

The three bolus doses tested of Diprivan® and B8 were 7.5, 10, and 15 mg/kg.

FIG. 8 provides a plot for Diprivan® with 15 ml kg^-1 Intralipid®. The data are plotted as time to recovery of righting reflex as a function of drug dose, expressed on a mg/kg basis for the propofol component of the nanoemul-

Statistics
sion. Using the slope of the trendline to represent rate of clearance, the lower the slope the more rapid the clearance of propofol from its effect site (faster recovery of righting reflex for a given dose).

The slope of the line using Diprivan® followed by Intralipid® is 39% less than the slope of the line using Diprivan® alone. This is a significant difference (p = 0.014). There was greater reduction in duration of anesthesia for higher doses (10, 15 mg/kg) and virtually no change for the 7.5 mg/kg dose.

FIG. 9 provides a plot for B8 with 15 ml kg⁻¹ Intralipid®. The data are plotted as time to recovery of righting reflex as a function of drug dose, expressed on a mg/kg basis for the propofol component of the nanoemulsion.

Again, a reduction (51%) in the slope of the trend line was seen using B8 with Intralipid®. This is significantly different (p = 0.046). However, most of this reduction was due to the 15 mg/kg dose with little, if any, reduction for the 7.5 and 10 mg/kg doses.

FIG. 10 provides a plot for B8 and Diprivan® with Intralipid®. The data are plotted as time to return of righting reflex vs Intralipid® dose. Large doses (15 mg/kg) of B8 and Diprivan® were administered in combination with decreasing doses of Intralipid® (15, 7.5, and 3.75 ml/kg). Error bars are added.

The 15 ml/kg dose of Intralipid® caused a significant reduction in duration of anesthesia for B8 (p = 0.0008), and a noticeable but not significant decrease for Diprivan® (p = 0.0632). The smaller doses (3.75 and 7.5 ml/kg) of Intralipid® cause little, if any, reduction compared to 15 mg/kg doses without the addition of Intralipid®.

Discussion

These novel fluoropolymer emulsions of propofol, L3, B8, and F8 were able to reliably induce anesthesia in rats. There were no ill effects either acutely or after more than 10 administrations over a 2-3 week period. The threshold dose of the emulsion containing only fluoropolymer and propofol, B8, was not significantly different than that of Diprivan® in rats; the threshold dose of L3 and F8 were only slightly higher. In regards to duration of anesthesia after a bolus dose, B8 and L3 were not significantly different across all doses. For higher doses (10 and 15 mg/kg) B8 and L3 produce a significantly shorter duration of anesthesia than Diprivan®, and F8 longer. This may be due to decreased bioavailability or slower release of propofol in the B8 and L3 emulsions, and especially in F8, compared to Diprivan®.

Interestingly, the formulation containing only propofol and Lipoid E80 did not cause LORR even at high doses. Additionally, the L3 emulsion, which contained Lipoid E80, required a higher threshold dose to cause LORR than B8, which did not contain the surfactant. If Lipoid E80 is a factor in the bioavailability of propofol from the emulsions, it may be possible to vary its concentration to affect release of the drug. This could have implications for pain on injection as well as hemodynamic stability after bolus dosing.

These 3 formulations of propofol all showed similar efficacy, potency, and duration in producing and maintaining anesthesia with bolus dosing. Additionally, clearance of propofol from its effect site can be accelerated with Intralipid® after an induction dose. This effect was observed even with the lipid-based formulation (Diprivan®), but was stronger for the lipid-free formulation B8. The effect was most significant when a high dose of drug (15 mg/kg) was followed by a high volume of lipid (15 ml/kg).

Several mechanisms have been proposed for lipid rescue in toxicity from bupivacaine as well as other drugs. The most commonly cited is via “partitioning” in which the lipid acts as an intravascular “sink,” causing decreased concentrations of drug at the effect site. A second proposed mechanism is the accelerated shunting of the drug to its site of metabolism, which is typically the liver for lipid-soluble drugs. (Weinberg/VadeBoncouer, Weinberg/Ripper) In either case, there is increased clearance of the drug from the effect site, which in the case of propofol is GABAα receptors in the CNS. We see this in the decreased slope of the linear regression lines when propofol administration is followed by Intralipid® bolus. Partitioning has been proposed as a mechanism for several lipid soluble drugs (local anesthetics, calcium channel blockers, beta blockers, etc.) whose toxicity has been treated with lipid infusion. (Jamaty, Perez) This could partially explain our results in that propofol, log P (octanol:water partition coefficient) 3.79 (Babu), is more lipid soluble than bupivacaine, which has a log P of 3.41. (Hausch)

It would follow then that a high lipid dose would shorten duration of anesthesia more than a lower dose, but we saw a lack of effect with 7.5 and 3.75 ml/kg doses of Intralipid®. There is some evidence that in bupivacaine toxicity, lipid works to reverse inhibition of fatty acid metabolism in cardiac muscle. (Weinberg) It may be possible that Intralipid® interferes with propofol binding to the GABAα receptor, and that there is a threshold concentration required to see this effect, which the 7.5 and 3.75 ml/kg doses are not large enough to reach.

The 15 ml/kg dose of Intralipid® that was found to be effective in this study is relatively large. However, it is possible that lower volumes would be effective in a human as compared to the rat. Induction of anesthesia in humans typically requires 1-2 mg/kg, but in rats that dose is 5-10 times higher. A similar reduction in Intralipid® dose to 1.5-3 ml/kg or less may have particular clinically utility.

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STATEMENTS REGARDING INCORPORATION BY REFERENCE AND VARIATIONS

All references cited throughout this application, for example patent documents including issued or granted pat-
The terms and expressions which have been employed herein are used as terms of description and not of limitation, and there is no intention in the use of such terms and expressions of excluding any equivalents of the features shown and described or portions thereof, but it is recognized that various modifications are possible within the scope of the invention claimed. Thus, it should be understood that although the present invention has been specifically disclosed by preferred, exemplary embodiments and optional features, modification and variation of the concepts herein disclosed may be resorted to by those skilled in the art, and that such modifications and variations are considered to be within the scope of this invention as defined by the appended claims. The specific embodiments provided herein are examples of useful embodiments of the present invention and it will be apparent to one skilled in the art that the present invention may be carried out using a large number of variations of the devices, device components, methods steps set forth in the present description. As will be obvious to one of skill in the art, methods and devices useful for the present methods can include a large number of optional composition and processing elements and steps.

When a group of substituents is disclosed herein, it is understood that all individual members of that group and all subgroups, including any isomers, enantiomers, and diastereomers of the group members, are disclosed separately. When a Markush group or other grouping is used herein, all individual members of the group and all combinations and subcombinations possible of the group are intended to be individually included in the disclosure. When a compound is described herein such that a particular isomer, enantiomer or diastereomer of the compound is not specified, for example, in a formula or in a chemical name, that description is intended to include each isomer and enantiomer of the compound described individual or in any combination. Additionally, unless otherwise specified, all isotopic variants of compounds disclosed herein are intended to be encompassed by the disclosure. For example, it will be understood that any one or more hydrogens in a molecule disclosed can be replaced with deuterium or tritium. Isotopic variants of a molecule are generally useful as standards in assays for the molecule and in chemical and biological research related to the molecule or its use. Methods for making such isotopic variants are known in the art. Specific names of compounds are intended to be exemplary, as it is known that one of ordinary skill in the art can name the same compounds differently.

It must be noted that as used herein and in the appended claims, the singular forms “a”, “an”, and “the” include plural reference unless the context clearly dictates otherwise. Thus, for example, reference to “a cell” includes a plurality of such cells and equivalents thereof known to those skilled in the art, and so forth. As well, the terms “a” (or “an”), “one or more” and “at least one” can be used interchangeably herein. It is also to be noted that the terms “comprising”, “including”, and “having” can be used interchangeably. The expression “of any of claims XX-YY” (wherein XX and YY refer to claim numbers) is intended to provide a multiple dependent claim in the alternative form, and in some embodiments is interchangeable with the expression “as in any one of claims XX-YY.”

Unless defined otherwise, all technical and scientific terms used herein have the same meanings as commonly understood by one of ordinary skill in the art to which this invention belongs. Although any methods and materials similar or equivalent to those described herein can be used in the practice or testing of the present invention, the preferred methods and materials are now described. Nothing herein is to be construed as an admission that the invention is not entitled to antedate such disclosure by virtue of prior invention.

Every formulation or combination of components described or exemplified herein can be used to practice the invention, unless otherwise stated.

Whenever a range is given in the specification, for example, a temperature range, a time range, or a composition or concentration range, all intermediate ranges and subranges, as well as all individual values included in the ranges given are intended to be included in the disclosure. As used herein, ranges specifically include the values provided as endpoint values of the range. For example, a range of 1 to 100 specifically includes the end point values of 1 and 100. It will be understood that any subranges or individual values in a range or subrange that are included in the description herein can be excluded from the claims herein.

As used herein, “comprising” is synonymous with “including,” “containing,” or “characterized by,” and is inclusive or open-ended and does not exclude additional, unrecited elements or method steps. As used herein, “consisting of” excludes any element, step, or ingredient not specified in the claim element. As used herein, “consisting essentially of” does not exclude materials or steps that do not materially affect the basic and novel characteristics of the claim. In each instance herein any of the terms “comprising”, “consisting essentially of” and “consisting of” may be replaced with either of the other two terms. The invention illustratively described herein suitably may be practiced in the absence of any element or elements, limitation or limitations which is not specifically disclosed herein.

One of ordinary skill in the art will appreciate that starting materials, biological materials, reagents, synthetic methods, purification methods, analytical methods, assay methods, and biological methods other than those specifically exemplified can be employed in the practice of the invention without resort to undue experimentation. All art-known functional equivalents, of any such materials and methods are intended to be included in this invention. The terms and expressions which have been employed are used as terms of description and not of limitation, and there is no intention that in the use of such terms and expressions of excluding any equivalents of the features shown and described or portions thereof, but it is recognized that various modifications are possible within the scope of the invention claimed. Thus, it should be understood that although the present invention has been specifically disclosed by preferred embodiments and optional features, modification and variation of the concepts herein disclosed may be resorted to by those skilled in the art, and that such modifications and variations are considered to be within the scope of this invention as defined by the appended claims.
We claim:
1. An emulsion for delivery of a therapeutic agent, said emulsion comprising:
   - an aqueous solution;
   - semi-fluorinated block copolymers; wherein each of said semi-fluorinated block copolymers independently comprises a hydrophilic block, a hydrophobic block and a fluorophilic block; wherein said hydrophobic block of each of said semi-fluorinated block copolymers is provided between said fluorophilic block and said hydrophilic block; wherein the semi-fluorinated block copolymers have a concentration selected from the range of 10 mg mL\(^{-1}\) to 50 mg mL\(^{-1}\);
   - said therapeutic agent comprising propofol; wherein the propofol has a concentration selected from the range of 0.2 mg mL\(^{-1}\) to 50 mg mL\(^{-1}\); and
   - a perhalogenated fluorour compound; wherein the perhalogenated fluorour compound is 5% to 20% by volume of said emulsion;
   - said emulsion comprising a continuous phase and a dispersed phase, wherein said continuous phase comprises said aqueous solution and said dispersed phase comprises said semi-fluorinated block copolymers, said therapeutic agent and said perhalogenated fluorour compound.
2. The emulsion of claim 1, wherein said fluorophilic block, said hydrophilic block, or both, of each of said semi-fluorinated block copolymers is a polymer terminating group.
3. The emulsion of claim 1, wherein said fluorophilic block, said hydrophilic block, or both, of each of said semi-fluorinated block copolymers is directly linked to said hydrophobic block.
4. The emulsion of claim 1, wherein said fluorophilic block, said hydrophilic block or both are independently linked to said hydrophobic block via a linker moiety selected from the group consisting of an ether group, a carbamate group, an amide group, an alkylene group, amino group or any combination of these.
5. The emulsion of claim 1, wherein each of said fluorophilic blocks of said semi-fluorinated block copolymers is independently a fluorocarbon moiety having between 3 to 31 carbon fluorine bonds.
6. The emulsion of claim 1, wherein said hydrophilic blocks of said semi-fluorinated block copolymers are independently selected from the group consisting of a polyoxygenated polymer block, a polysaccharide block, a chitosan block and a poly(ethylene glycol) block.
7. The emulsion of claim 1, wherein each of said hydrophilic blocks of said semi-fluorinated block copolymers is independently selected from the group consisting of a \(C_{x-}C_{z+}\) alkylene group, a poly(\(\varepsilon\)-caprolactone) block, a polylactic acid block, a poly(propylene glycol) block, a poly(aminic acid) block, a poly(ester) block and polylactico-glycolic acid).
8. The emulsion of claim 1, wherein each of said semi-fluorinated block copolymers independently has the formula (FX2):

   \[
   \text{R}^{1}\text{O} \to \text{L}^{1}\eta_{1} \to \text{C}_{2} \theta_{1} \to \text{C}_{2} \theta_{1} \to \text{CF}_{2} \eta_{1} \to \text{R}^{2};
   \]
   
   wherein \(m\) is 0 or 1 and \(n\) is 0 or 1;
   
   wherein \(q\) is an integer selected from the range of 10 to 300, \(o\) is an integer selected from the range of 5 to 20, and \(p\) is an integer selected from the range of 3 to 15;
   
   wherein \(R^{1}\) is hydrogen, methyl, \(C_{x-}C_{z+}\) alkyl, \(C_{x-}C_{z+}\) cycloalkyl, \(C_{x-}C_{z+}\) aryl, \(C_{x-}C_{z+}\) heteroaryl, \(C_{x-}C_{z+}\) alkoxy or \(C_{x-}C_{z+}\) acyl;
   
   wherein \(R^{2}\) is hydrogen, halo or \(C_{x-}C_{z+}\) alkyl;
   
   wherein each of \(L^{1}\) and \(L^{2}\) is independently \(-\text{(CH}_{2}\text{)}_{o}(-\text{O})_{e}\text{(CH}_{2}\text{)}_{p}(-\text{S})_{o}\text{(CH}_{2}\text{)}_{p}\)
   
   \(-\text{(CH}_{2}\text{)}_{o}(-\text{NR})_{e}\text{(CH}_{2}\text{)}_{p}(-\text{COO})_{o}\text{(CH}_{2}\text{)}_{p}\)
   
   or
   
   \(-\text{(CH}_{2}\text{)}_{o}(-\text{NR})_{e}\text{(CH}_{2}\text{)}_{p}\text{COO})_{o}\text{(CH}_{2}\text{)}_{p}\)

9. The emulsion of claim 8, wherein each of said semi-fluorinated block copolymers independently has the formula (FX4A) or (FX4B):

   (FX4A)

   \[
   \text{H}_{3}\text{C} \to \text{O} \to \text{O} \to \text{H}_{2}\text{O} \to \text{H}_{2}\text{O} \to \text{H}_{2}\text{O} \to \text{F} \quad \text{or} \quad \text{H}_{3}\text{C} \to \text{O} \to \text{O} \to \text{H}_{2}\text{O} \to \text{H}_{2}\text{O} \to \text{H}_{2}\text{O} \to \text{F}.
   \]

10. The emulsion of claim 8, wherein each of said semi-fluorinated block copolymers independently has the formula (FX5A) or (FX5B):

   (FX5A)

   \[
   \text{H}_{3}\text{C} \to \text{O} \to \text{O} \to \text{H}_{2}\text{O} \to \text{H}_{2}\text{O} \to \text{H}_{2}\text{O} \to \text{F} \quad \text{or} \quad \text{H}_{3}\text{C} \to \text{O} \to \text{O} \to \text{H}_{2}\text{O} \to \text{H}_{2}\text{O} \to \text{H}_{2}\text{O} \to \text{F}.
   \]

11. The emulsion of claim 1, wherein said perhalogenated fluorour compound is selected from the group consisting of perfluorooctyl bromide, perfluorononyl bromide, perfluoredecyl bromide, perfluoroedecalin, perfluorooctlchloro, bis-perfluorobutyl ethylen and perfluoro(methyldecalin).

12. The emulsion of claim 1, wherein said dispersed phase comprises a plurality of droplets dispersed in said continuous phase, wherein said droplets have an average diameter less than or equal to 400 nanometers.

13. The emulsion of claim 1, wherein said droplets have a fluorophilic core comprising said fluoropholic blocks of said semi-fluorinated block copolymers; a hydrophobic exterior shell comprising said hydrophobic blocks of said semi-fluorinated block copolymers; and a hydrophobic intermediate shell comprising said hydrophobic blocks of said semi-fluorinated block copolymers.

14. A method of delivering a therapeutic agent to a subject in need thereof, said method comprising the steps of:
   
   providing an emulsion comprising:
   
   an aqueous solution;
   
   semi-fluorinated block copolymers; wherein each of said semi-fluorinated block copolymers independently comprises a hydrophilic block, a hydrophobic
block and a fluorophilic block; wherein said hydrophobic block of each of said semi-fluorinated block copolymers is provided between said fluorophilic block and said hydrophobic block; wherein the semi-fluorinated block copolymers have a concentration selected from the range of 10 mg mL\(^{-1}\) to 50 mg mL\(^{-1}\);

said therapeutic agent comprising propofol; wherein the propofol has a concentration selected from the range of 0.2 mg mL\(^{-1}\) to 50 mg mL\(^{-1}\); and a perhalogenated fluorous compound; wherein the perhalogenated fluorous compound is 5% to 20% by volume of said emulsion;

said emulsion comprising a continuous phase and a dispersed phase, wherein said continuous phase comprises said aqueous solution and said dispersed phase comprises said semi-fluorinated block copolymers, said therapeutic agent and said perhalogenated fluorous compound; and

administering said emulsion to said subject, wherein said therapeutic agent is released from said emulsion thereby delivering said therapeutic agent to said subject in need thereof.

15. The method of claim 14, wherein said step of administering said emulsion provides for controlled release of said propofol from said emulsion.

16. The method of claim 14, wherein said step of administering said emulsion is carried out via intravenous injection.

17. The method of claim 14, wherein a volume of said emulsion is less than or equal to 500 mL is administered to said subject.

18. The method of claim 14, wherein said emulsion is delivered to said subject at a rate less than or equal to 100 mL per minute.

19. A method of making an emulsion, said method comprising the steps of:

providing a therapeutic formulation comprising:
an aqueous solution;

semi-fluorinated block copolymers; wherein each of said semi-fluorinated block copolymers independently comprises a hydrophilic block, a hydrophobic block and a fluorophilic block; wherein said hydrophobic block of each of said semi-fluorinated block copolymers is provided between said fluorophilic block and said hydrophilic block; wherein the semi-fluorinated block copolymers have a concentration selected from the range of 10 mg mL\(^{-1}\) to 50 mg mL\(^{-1}\);

said therapeutic agent comprising propofol; wherein the propofol has a concentration selected from the range of 0.2 mg mL\(^{-1}\) to 50 mg mL\(^{-1}\); and a perhalogenated fluorous compound; wherein the perhalogenated fluorous compound is 5% to 20% by volume of said emulsion; and

emulsifying said therapeutic formulation, thereby making an emulsion comprising a continuous phase and a dispersed phase, wherein said continuous phase comprises said aqueous solution and said dispersed phase comprises said semi-fluorinated block copolymers, said therapeutic agent and said perhalogenated fluorous compound.

20. The method of claim 19, wherein said step of emulsifying said therapeutic formulation comprises the steps of:

adding said propofol and said perhalogenated fluorous compound to said aqueous solution having said semi-fluorinated block copolymers therein, thereby generating a mixture; and

homogenizing said mixture, thereby generating said emulsion.

21. The method of claim 19 further comprising the step of lowering a temperature of said mixture during said step of homogenizing said mixture.

* * * * *